SUPPLEMENTARY MATERIAL

Propofol Detection and Quantification in Human Blood: The Promise of Feedback Controlled, Closed-loop Anesthesia

Francine Kivlehan^a, Edward Chaum^b, Ernö Lindner^a

 ^a Department of Biomedical Engineering, University of Memphis, Memphis, Tennessee 38152
^b Departments of Ophthalmology and Biomedical Engineering, University of Tennessee Health Science Center, Memphis, Tennessee 38152



Figure S1: Schematic representation of the surface profiler scans over a partially membrane-coated glass cover slip (left) and the recorded surface profiles (right).



Figure S2: CA transients recorded with a PVC membrane-coated GC sensor following the injection of 175 μ L propofol standards (1.00 μ M and 12.00 μ M, with 5% BSA content) and HSA samples with 6.00 μ M nominal propofol concentration into a continuously flowing PBS buffer solution.

The results of the standard addition measurements were calculated using the following equation:

$$c_s = \frac{c_{St}V_{St}}{\frac{i_{2corr}}{i_{1corr}}(V_s + V_{St}) - V_s}$$
Eq. S1

where c_s is the sample concentration, c_{St} is the concentration of the standard, V_s is the sample volume, V_{St} is the volume of the standard, and i_{1corr} and i_{2corr} are background current corrected current values measured in the sample before and after the addition of the standard, respectively.



Figure S3: CA response of a membrane-coated GC working electrode on the external surface of a catheter prototype to propofol injectable emulsion in PBS in combination with an external reference and counter electrodes Inset: Calibration curves constructed from the corresponding steady state current and concentration values.