

1 **Microfluidic device for multiplexed detection of fungal infection biomarkers in**
2 **grape cultivars**

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16 **S1 – Jasmonic acid – BSA conjugation**

17 In this work, a conjugation between jasmonic acid (JA) and bovine serum albumin (BSA) is performed in
18 order to immobilize JA on the microbead surface. To confirm the conjugation of JA to the BSA molecules,
19 both were incubated at 5 g/L with the silica microbeads for 1h under constant agitation. Then, both
20 functionalized beads were packed into a micro-column and the labelled α -JA antibody was injected for 5
21 min at a concentration of 50 mg/L at a flow rate of 1 μ L/min, followed by a 1 min washing step with PBS
22 at 5 μ L/min. The results obtained are presented in Figure S1.

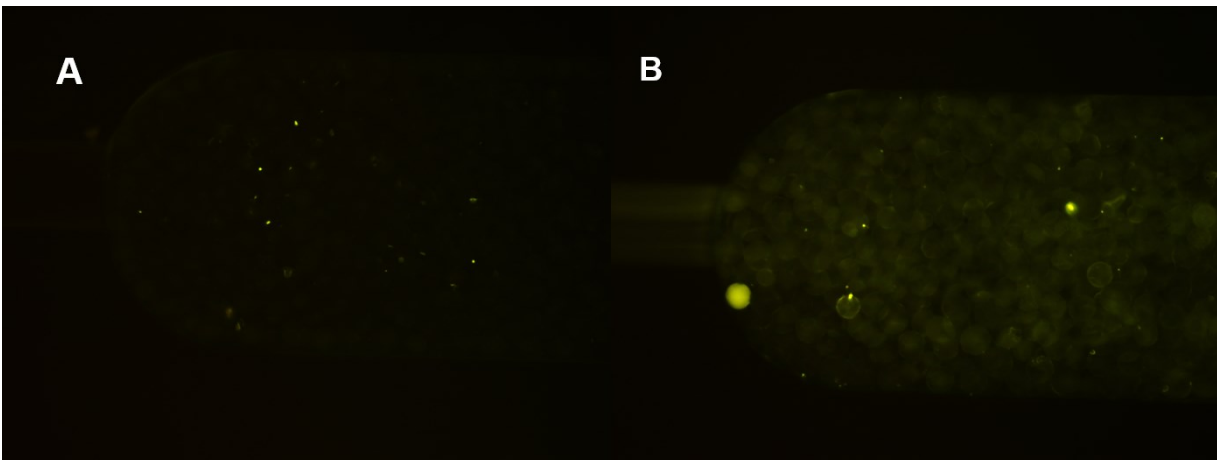


Figure S1 – Results obtained concerning the interaction between the α -JA antibody with microbeads functionalized with BSA (A) and JA-BSA (B). Pictures were enhanced for visualization purposes.

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24 The results presented demonstrate that the antibody does not interact with the BSA functionalized beads,
25 however it does attach to the JA-BSA beads. These results also motivated the use of BSA as the blocking
26 agent of the assay.

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28 **S1 – Photosensor Characterization**

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30 In this work, a thin-film amorphous silicon photosensor array is used as an optical transducer for the
31 different detection methods used. The active layer of the sensor is a 200 μ m x 200 μ m and is composed
32 of a 500 nm thick layer of intrinsic hydrogenated amorphous silicon. The deposition conditions for the film
33 using an Oxford Plasma Pro 100 were: Temperature= 300 $^{\circ}$ C, Chamber Pressure= 350 mTorr, RF Power=
34 10 W, SiH₄ flow rate= 25 sccm, H₂ flow rate= 10 sccm, Deposition time= 21 min. The *I*-*V* curve as well as

35 the photoresponse of the sensors at the wavelengths of interest for the absorbance assays are shown in
36 Figure S2.

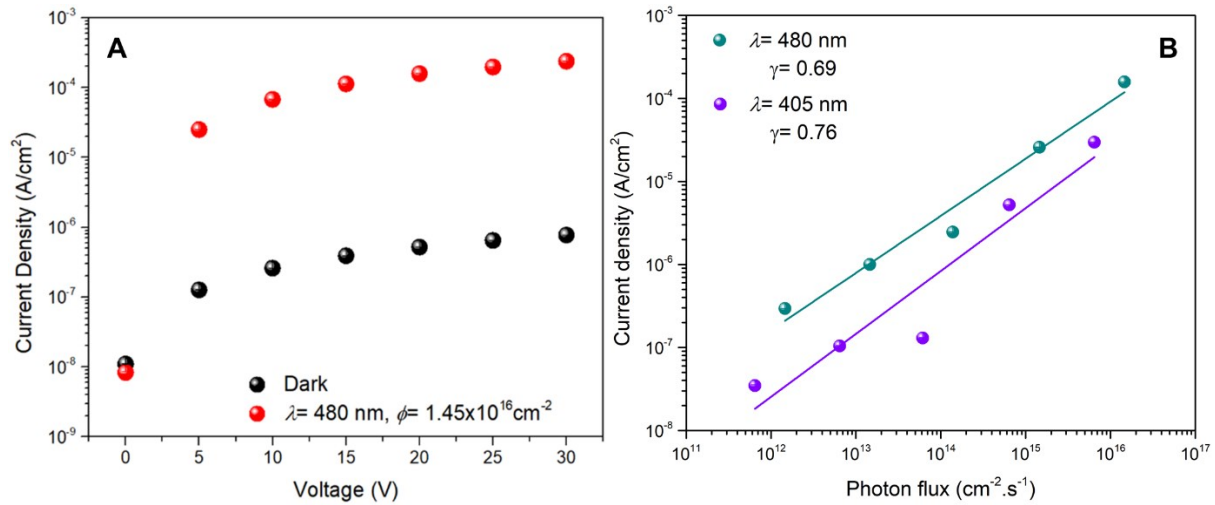


Figure S2– (A) *I*-*V* curves in the dark and in a condition of high light. (B) Photoresponse curves for the wavelengths of interest for the detection of SA ($\lambda= 405$ nm) and AzA ($\lambda= 480$ nm). The slope of the fit, γ , is correlated to the generation rate of the sensor.

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38 For the detection of the fluorescent signal in the jasmonic acid assay, it is necessary to block out the
39 excitation light at $\lambda= 405$ nm, while maximizing the transmission of the emitted light at $\lambda= 540$ nm. To do
40 this, a 1.5 μm thick silicon carbide high-pass filter was deposited on top of the sensor for this assay. The
41 transmission curve of the filter is presented in Figure S3.

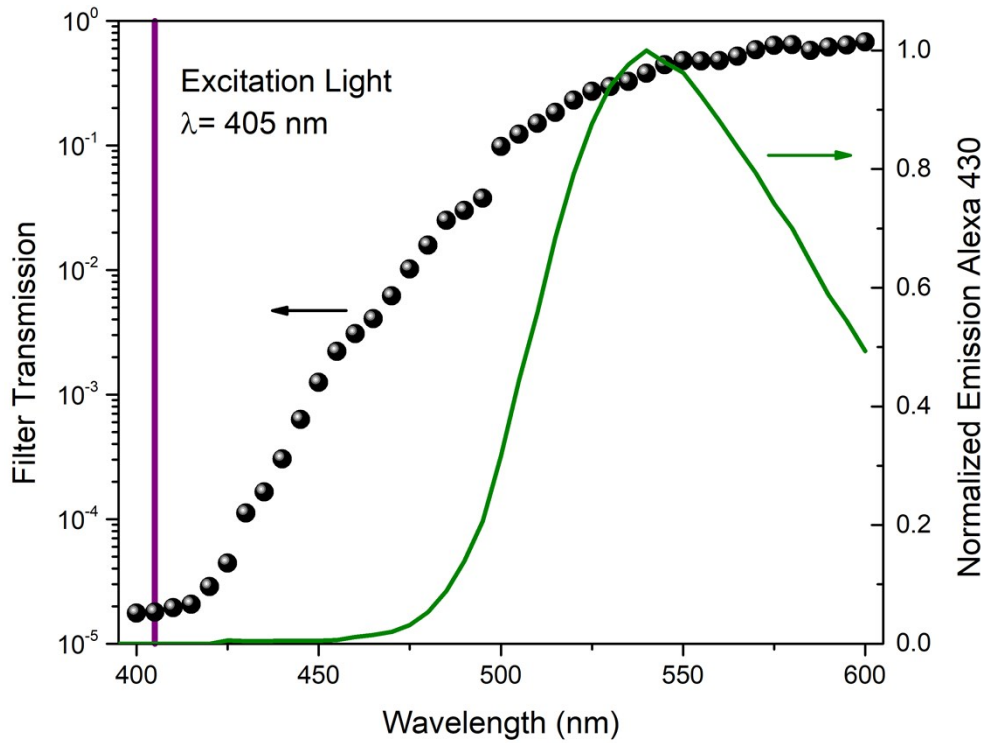


Figure S3 – Overlap of the silicon carbide filter transmission profile (Black dots) with the emission profile of the Alexa 430[®] fluorophore provided by the manufacturer (Green line). The excitation light source used was a $\lambda = 405 \text{ nm}$ laser.

42 To confirm that the a-SiC:H layer did not hinder the performance of the sensor, the photoresponse at $\lambda =$
 43 540 nm, which is the emission maximum of the Alexa 430[®] fluorophore, was performed and is presented
 44 in Figure S4.

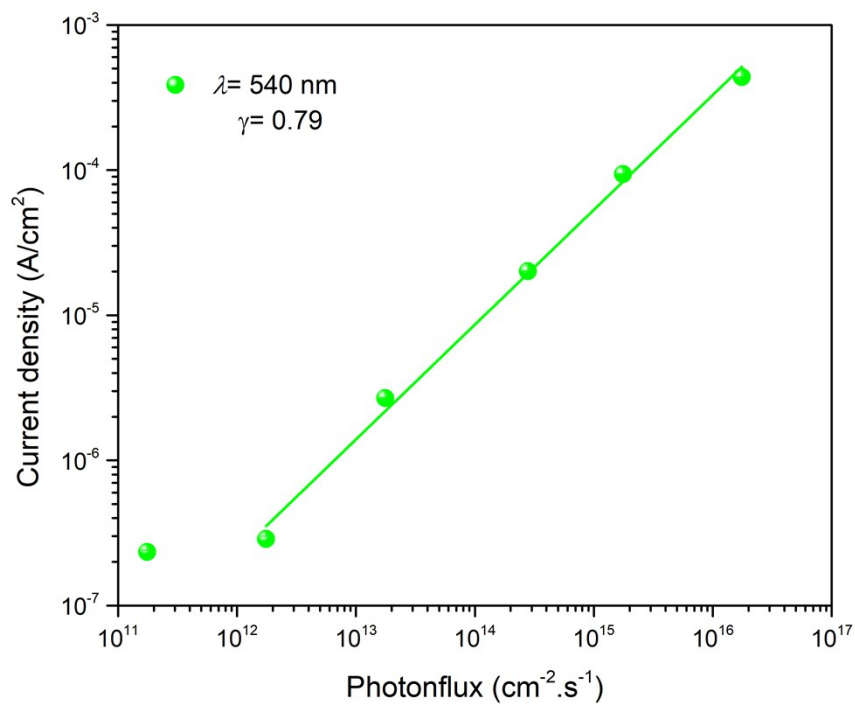


Figure S4 - Photoresponse curve for the wavelength of interest for the detection of JA ($\lambda = 540$ nm) using the a-SiC:H-filtered photoconductor. The slope of the fit, γ , is correlated to the generation rate of the sensor

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47 **S3 – SA Assay Absorbance Behavior**

48 To determine the optimal wavelength for the detection of SA through the complexation reaction with the
49 TiO_2 nanoparticles, the absorbance spectrum of free SA, free TiO_2 and the product of reaction were
50 measured and are presented in Figure S5.

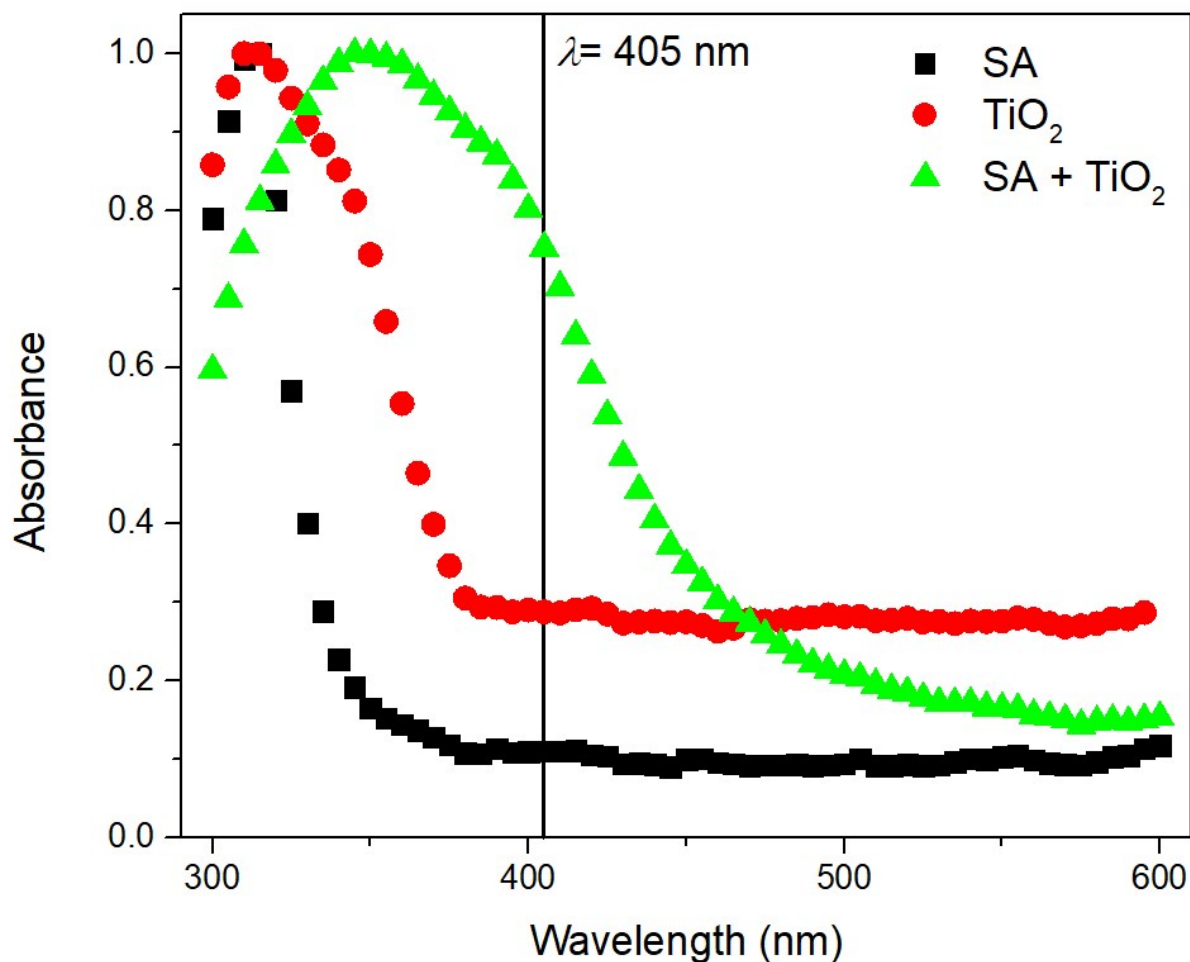


Figure S5 – Absorbance spectra of free SA (black), free TiO₂ nanoparticles (red) and the product of the reaction (green). The shift in absorbance from the UV range into the visible due to the reaction is visible here. The vertical line at $\lambda = 405$ nm represents the chosen wavelength for the assay.

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52 S4 – TiO₂ Interference assays

53 Since the assay for the detection of AzA is directly downstream to the chamber for the detection of SA,
 54 there is the possibility that the TiO₂ nanoparticles could seep through the first chamber and interfere with
 55 the detection of AzA. To determine if any interferences were present, known concentrations of AzA and
 56 TiO₂ were mixed together and tested using the AzA enzymatic assay. These results are presented in Figure
 57 S6.

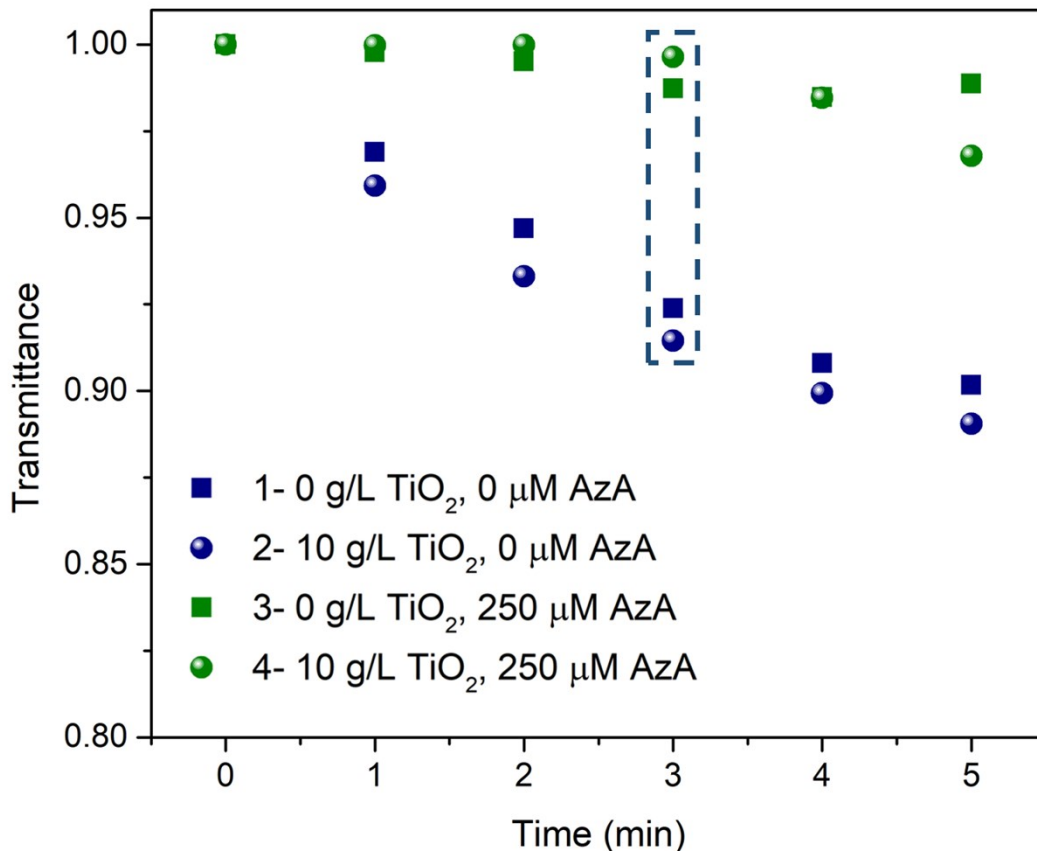


Figure S6 – Assays performed to determine the existence of interference from the TiO₂ nanoparticles on the enzymatic activity of tyrosinase.

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59 By analyzing the results presented in Figure S6, it is possible to determine that there is no interference
 60 caused by the TiO₂ nanoparticles on the detection assay for AzA. In Figure S7 the interference caused by
 61 the presence of inorganic salts when mixed with the TiO₂ nanoparticles is demonstrated by using
 62 phosphate buffer saline (PBS) and compared to the results using DI-water and a SA solution in water.

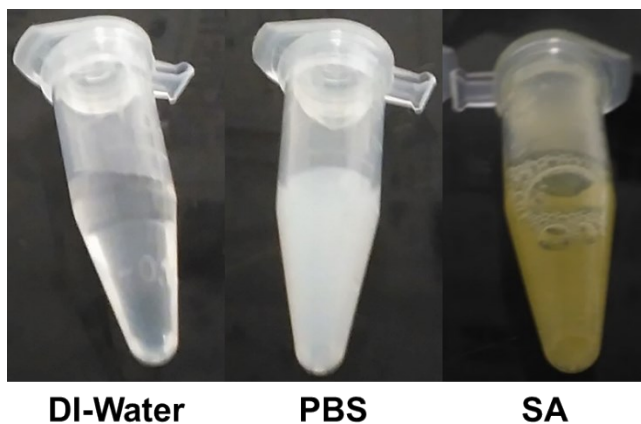


Figure S7 – Result of mixing the TiO₂ nanoparticles with DI-water, PBS and SA. It is important to notice the turbidity caused by the presence of PBS.

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