

## Supporting Information

### **A 3D printable perfused hydrogel vascular model to assay ultrasound-induced permeability**

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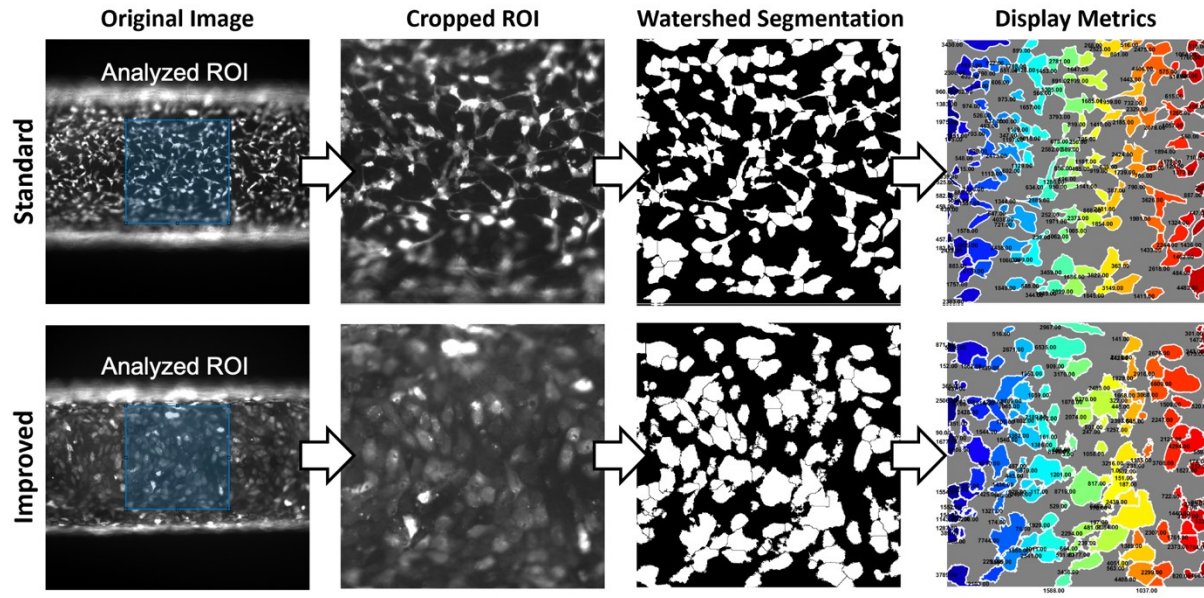
\* Authors contributed equally

**Movie S1. Representative time-lapse of a perfusion-permeability study for an improved endothelialized gel.** An endothelialized channel perfused with 70 kDa Rhodamine-Dextran at 100  $\mu\text{L min}^{-1}$  and subjected to 5 minutes of ultrasound at 2.0  $\text{W cm}^{-2}$ .

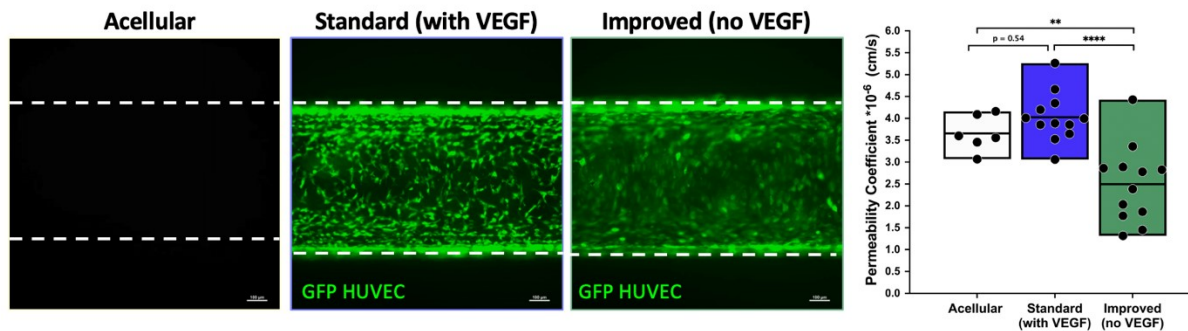
**Movie S2. Demonstration of custom MATLAB permeability GUI.** Video demonstrates the use of the permeability GUI to determine permeability coefficients, endothelialized channel behavior, and dye diffusion.

**Movie S3. Time-lapse of VE-Cadherin-GFP HUVECs in response to ultrasound with no microbubbles.** An endothelialized gel was subjected to ultrasound of power intensity 2.0  $\text{W cm}^{-2}$  for 5 min with 5 min of perfusion prior to ultrasound and after ultrasound collected for a total acquisition time of 15 minutes.

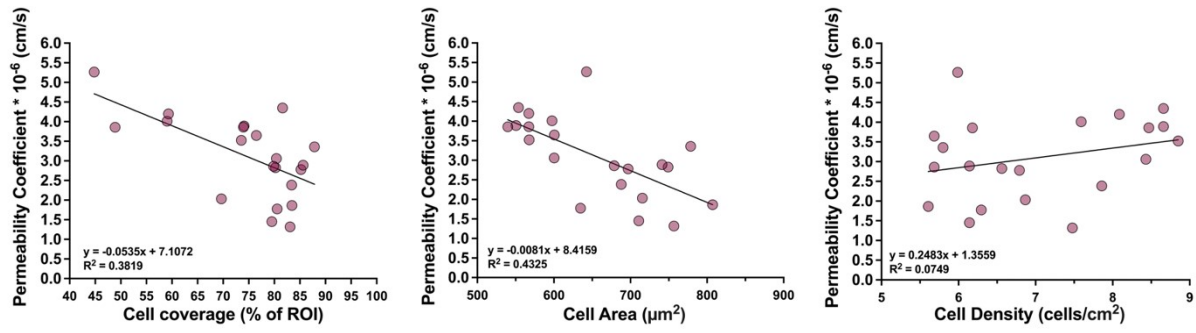
**Movie S4. Time-lapse of VE-Cadherin-GFP HUVECs in response to ultrasound with microbubbles.** An endothelialized gel was subjected to ultrasound of power intensity 2.0  $\text{W cm}^{-2}$  for 5 min with 5 min of perfusion prior to ultrasound and after ultrasound collected for a total acquisition time of 15 minutes.



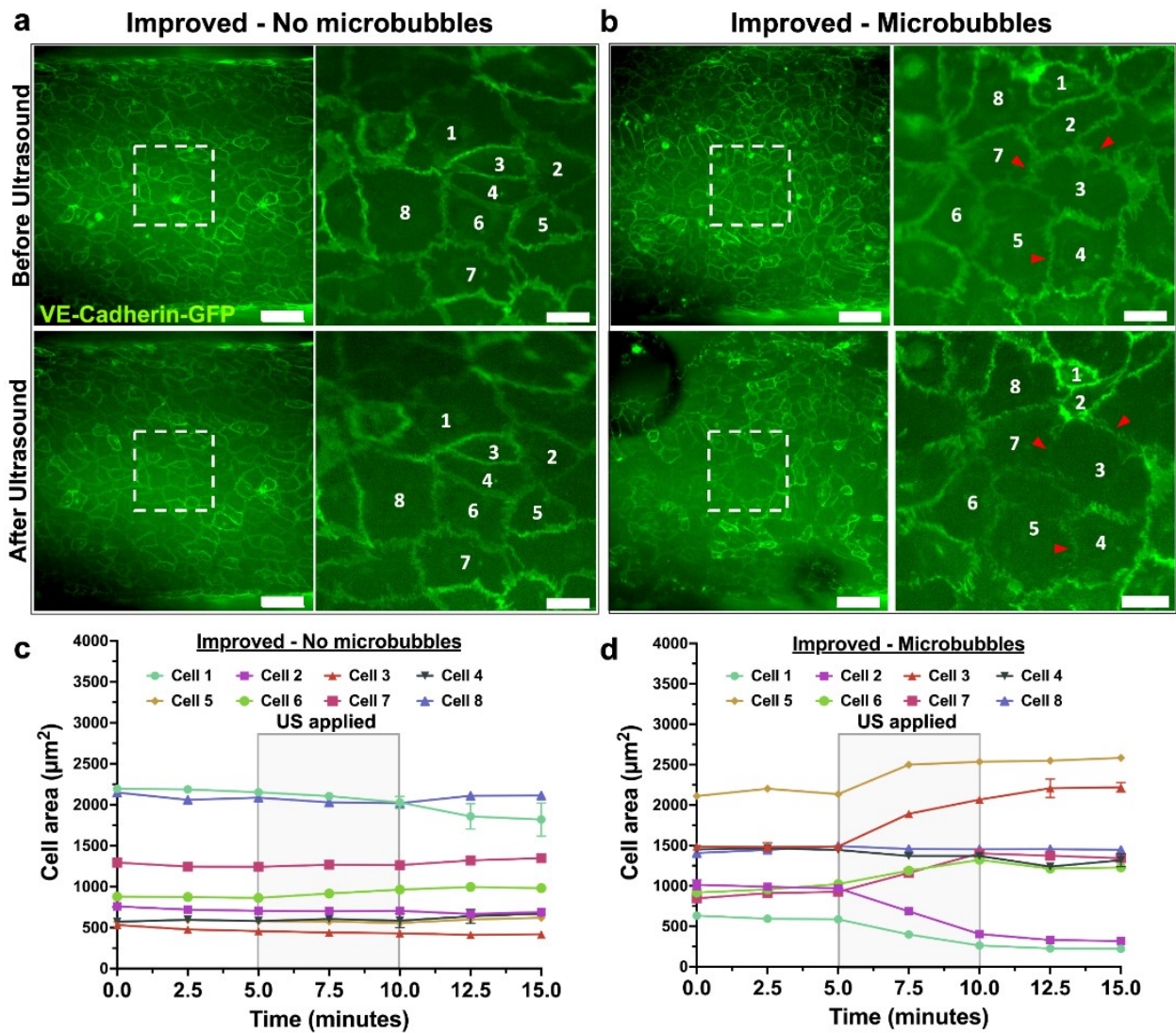
**Figure S1. Workflow for quantification of cell morphology shown in Figure 1.** Image quantification utilizes a custom MATLAB script and begins with importing the high-resolution TIFF, cropping to a desired ROI, performing a watershed segmentation, and then producing metrics such as cell coverage, cell area, and cell density for the ROI.



**Figure S2. Permeability of acellular, standard, and improved gels before ultrasound application.** Permeability was determined using 70 kDa Rhodamine-Dextran and the custom MATLAB GUI detailed in this manuscript. To utilize the GUI's edge tracking feature, 150 kDa FITC-Dextran was used to track the edges of the channels in the acellular trials when GFP HUVECs are not present. 150 kDa FITC-Dextran was able to be used as it will not diffuse through the gel in the timeframe of the acquisition. The resulting permeability coefficients showed a statistical significance (\*\*\*\*) between the standard (n=12) and improved groups (n=12), as well as showing statistical significance (\*\*) between the acellular (n=6) and the improved group. No statistical significance was seen between the acellular and standard groups. Significance was determined using a one-way ANOVA followed by Tukey's multiple comparisons test (Tukey-Kramer to adjust for unequal number of replicates), \* $p < 0.05$ , \*\* $p < 0.01$ , \*\*\*\* $p < 0.0001$ .



**Figure S3. Linear regression of permeability coefficient correlations.** A simple linear regression was performed on the data shown in Figures 3e-3g where the red circles are points from both the standard and improved groups.



**Figure S4. VE-Cadherin-GFP HUVECs enable the visualization of cell-cell junction (VE-Cadherin) dynamics in living cells under the application of ultrasound.** VE-Cadherin-GFP HUVECs were seeded at  $30 \text{M mL}^{-1}$  within the vascular hydrogel model and underwent perfusion culture at  $5 \mu\text{L min}^{-1}$  (improved condition, VEGF removed). During the study, perfusate (left (a, c): no microbubbles, right (b, d): with microbubbles) was perfused through the endothelialized channel at  $100 \mu\text{L min}^{-1}$ . Panels a & b show representative images of the endothelial cell-cell junctions before and after applying ultrasound at  $2.0 \text{ W cm}^{-2}$  for 5 minutes (same conditions used with GFP HUVEC studies) with red arrowheads indicating disrupted junctions, scale bars,  $100 \mu\text{m}$  and  $25 \mu\text{m}$  (insets). Graphs c & d display cell area over time of eight individual cells (denoted in a & b insets before and after ultrasound) with a box indicating when ultrasound is applied.