1	Biodegradable smart materials with self-healing and							
2	shape memory function for wound healing							
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9	Chen)							
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15 16 17 18	Fig. S1 Mechanical properties of the $P_3$ : (a) The Storage modulus (G', solid line) and loss modulus(G", dotted line) of the $P_3$ vs. frequency at room temperature; (b) The G' and G" of the $P_3$ vs.temperatureatafixedfrequencyofHz							
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24	the 5 th days after the surgery.	 39
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## 25 S1. Experimental Section

### 26 Materials

2, 2-Bis(hydroxymethyl) propionic acid (99%) was purchased from Tianjin Bodi Chemical Co., Ltd.
(Tianjin, China). Benzyl chloride (99%) was purchased from Shanghai Chemical Reagent plant
(Shanghai, China). Methoxypolyethylene glycols (mPEG<sub>113</sub>, 5.0 kDa) was purchased from Alpha
chemical co., Ltd. Triethylamine (99%) was purchased from Tianjin Damao Chemical Reagent
Factory. (Tianjin, China). Stannous octoate [Sn(Oct)<sub>2</sub>] (99%) was purchased from SigmaAldrich.
Other solvents were obtained from commercial sources and used as received.

33 Ethics statement: Only volunteer blood donor was included. She was specifically informed that the
34 obtained materials would be tested for hemolysis test. Meanwhile, she offered signed written
35 informed consent.

The synthesis of monomer and the self-healing elastomer: The monomer was synthesized 36 according to our previous work. <sup>[1]</sup> It is noted that the monomer 2-methyl-2-benzyloxy carbonyl 37 38 propylene carbonate (MBC), the mPEG<sub>113</sub> and Sn(Oct)<sub>2</sub> are deemed as a hydrophobic monomer (denoted as M), a macromolecular initiator (denoted as I), and a catalyst (denoted as C), 39 respectively. The detail was described as follows: mPEG<sub>113</sub>, MBC and stannous octoate were put 40 41 into a dried silanized glass ampoule proportionally (Table S1). The ampoule was evacuated, purged with nitrogen three times, and sealed. Then kept the ampoule in an oil bath at 85°C for 24 h. After 42 polymerization, the as-prepared organogels were swelled in a large amount of methylene chloride 43 for 48 h to dissolve unreacted monomer. Then, products were shrunken in ethanol for 24 h and 44 shrank products were dried in a vacuum oven for four days to constant weight. Special note: before 45

46 the experiment, Teflon mold was put into the polymerization tube to ensure product molding, and

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47 the resultant elastomers were named as  $P_1$ - $P_3$ .

49 Note: " $\times$ " will not be the formation of gelation, and " $\sqrt{}$ " will be the formation of gelation

samples	M:I	M:C	reaction time /h	reaction temperature /ºC	whether gel
<b>P</b> <sub>1</sub>	2000:1	500:1	24	100	$\checkmark$
$P_2$	2000:1	600:1	24	100	$\checkmark$
P <sub>3</sub>	2000:1	800:1	24	100	

50 **The self-healing behavior of the elastomers:** The repeatability tests are carried out in order to 51 accurately quantify the self-healing efficiency, and the obtained elastomers square (5.000 52 mm×5.000 mm) were cut into three completely separate pieces. At least three parallel samples were 53 recorded for each sample, using a surgical blade. Then, the self-healing of every sample has been

54 completely cut and have applied a slight force to dock softly the two cut interfaces.

Structure and thermal behavior characterization: Unless otherwise noted, all tests are measured 55 at room temperature, and at least three parallel samples are recorded for each sample. FT-IR spectra 56 are determined on a PerkinElmer Spectrum One (B) spectrometer (PerkinElmer, Foster City, CA, 57 USA) over the wavenumber ranging from 4000 to 500 cm<sup>-1</sup>. The differential scanning calorimetry 58 (DSC) is carried out with a NETZSCH DSC-204 thermal analyzer (Netzsch, Hanau, Germany), the 59 measurements are obtained over a temperature range from -50 to 200 °C at a rate of 10 °C/min under 60 flowing nitrogen. The thermal decomposition temperatures are performed under a nitrogen 61 atmosphere with a Netzsch 209C TGA (Netzsch, Hanau, Germany) at a heating rate of 20 °C/min. 62 Mechanical properties characterization: All tests were performed on a universal test machine 63 64 (AGS-X, Shimadzu, Japan) with a 2000 N load cells. For tensile strength studies, all tests were performed at a constant speed of 10 mm/min at room temperature, at least five parallel samples were 65 66 recorded for each sample.

67 Self-healing tests: Optical microscope is used to observe the self-healing processes (Smartzoom 5, 68 Beijing, China) to record the changes of the scratch-width track. The procedure of self-healing at 69 room temperature, without requiring any external stimuli. The self-healing ability is monitored by 70 the detection of mechanical properties embracing modulus. Healing efficiency (HE) of elastomers 71 can be defined as the ratio of the stress or modulus of the healed ( $M_h$ ) and pristine elastomer ( $M_p$ ): 72 HE= ( $M_h/M_p$ ) eqn. 1 <sup>[4]</sup>

Shape memory performance. To qualitatively evaluate the shape memory properties and 73 temperature responsiveness, P<sub>1</sub>-P<sub>3</sub> were made into 3 cm rod-shaped materials. The plasticity was U-74 shaped under external force, and at least three parallel samples were recorded for each sample. The 75 detailed preparation is shown as follows: the obtained elastomers were put into 7 °C ice water to fix 76 shape for 10 s, and a 10 g weight was loaded for 10 s without deformation. Then, the fixed shape 77 78 was immersed in 37 °C water for 10 s. To calculate the shape fixity  $(R_f)$ :  $R_f = (180-\alpha)/180$  eqn. 2 and shape recovery  $(R_r)$ :  $R_r = \frac{180 - \alpha - \beta}{180 - \alpha}$  eqn. 3, where  $\alpha$  is the recovery angle, 180- $\alpha$  the fixed 79 temporary angle,  $\beta$  the residual angle. <sup>[5]</sup> 80

# 81 Enzymatic degradation

Enzymatic degradation of the obtained elastomer was carried out in lipase solutions
(Aspergillus oryzae,≥100,000 U/g) were purchased from Sigma-Aldrich) at 37 °C. The samples cut
into a cylindrical structure (ca. 3 mm (L)×2.000 mm (D)), and was put into a clean transparent
colorimetric tube. Then, 200 µL of enzyme solution were added into the tube, and the fresh enzyme
solution was exchanged every three days. The tube were incubated at 37 °C with constant shaking.
Furthermore, the extent of biodegradation was expressed in terms of weight loss percentage (eqn.
The loss weight ratio (%)=(m<sub>d</sub>-m<sub>i</sub>)/m<sub>i</sub>, where m<sub>d</sub> is the dried weight of after degradation, while

89 m<sub>i</sub> is the initial weight. Special note: before the fresh enzyme solution was put into the tube, the
90 sample was rinsed deionized water for three times.

#### 91 **Biological recognition**

In Vitro Cell Compatibility Test. The experiments of cell counting kit-8 (CCK-8) and clone-92 forming were used to evaluate the effect of the obtained materials on cell viability. The cell 93 compatibility of the obtained elastomer was performed in vitro.<sup>[6]</sup> The cell culture experiments were 94 determined by Human umbilical vein endothelial cells (HUVEC), which were purchased from the 95 Cell Bank of Chinese Academy of Sciences Type Culture Collection Committee (Shanghai, China). 96 Firstly, the HUVEC cells were digested, then centrifuged and counted. The HUVEC cells were 97 cultured in Dulbecco's modified Eagle medium (Gibco) contained 1% penicillin-streptomycin 98 solution (Gibco) and 10% fetal bovine serum (Gibco) in an incubator at 37 °C/5% CO<sub>2</sub>. Special 99 100 note: all of the materials were cut into a cylindrical structure ( thickness of 1 mm, diameter of 6 mm) and sterilized by 75% ethanol for one night and washed with phosphate buffer saline (PBS). 101

102 Subsequently, the sterilized samples were put into a 96-well plate. 1 mL HUVEC with a density of 8×105 cells/mL was seeded on them. The HUVEC cells were incubated in a thermostatic 103 incubator at 37 °C for 1 and 3 days, respectively. After the treatment, culture media was removed 104 and fresh media (500 µL) containing 2-(2-methoxy-4-nitrophenyl)-3-(4-nitrophenyl)-5-(2,4-105 106 disulfonic acid benzene)-2H-tetrazole monosodium salt (CCK-8) solution (100 µL, 5 mg/mL) was 107 placed into each well to further incubate at 37 °C for 4 h. Finally, the absorbance of the solution was measured at 450 nm by a microplate reader (ThermoFisher Scientific). Meanwhile, to 108 109 investigate the morphology of the cell proliferation on the specimens, the HUVECs cells after 3 110 days of incubation were stained with calcein AM (A017, USA) for 20 min. Then, the cells were 111 gently washed with PBS for third, and the spreading and attachments of cell on the specimens were

112 observed by the confocal laser scanning microscope (Eclipse Ts2-FL, Nikon, Japan).

Clone-forming experiments. The HUVEC cells in the logarithmic growth phase were used to 113 centrifuge and count the cells. Then, the cells were inoculated at 2000 cells/well in a 6-well plate, 114 and were drew cross to make the cells in the well plate evenly dispersed. The cells were placed into 115 116 an incubator for regular observation. After 3-5 days, when the appearance of obvious colonies were found, the well plate was removed to terminate the culture. After carefully removing the culture 117 solution, the culture media was rinsed thoroughly with PBS for 3 times. Then, the Coomassie 118 Brilliant Blue staining fixative solution was added to stain at room temperature for 10 min. Discard 119 the staining solution, the deionized water was used to rinse for third and dry at room temperature. The 120 inverted phase contrast microscope (DMIL-PH1, Leica, Germany) was used to observe the clone-121 122 forming condition of cells.

Blood Compatibility. The erythrocyte compatibility of the elastomers can be studied by the 123 hemolysis test. <sup>[7]</sup> First, 5 mL of the volunteer's blood was added into 10 mL of physiological saline 124 125 that does not contain calcium and magnesium ions. Then, the obtained saline containing the volunteer's blood was centrifuged at 2000 rpm for 10 min to obtain red blood cells (RBCs). The 126 RBCs were diluted into physiological saline with a final volume of 100 mL for later use. Secondly, 127 128 1 mL of the RBC suspension was introduced into the sample immersed in deionized water and 129 physiological saline (sodium chloride solution), and incubated at 37°C for 3 h, and then the RBCs were named as the positive control and negative control, respectively. Finally, the suspensions were 130 incubated in a shaking incubator at 37°C for 3 h, and then centrifuged at 8000 rpm for 5 min. The 131 132 absorbance of the released hemoglobin in the suspension is measured by the UV-Vis

133 spectrophotometer (UV-Eppendorf AG, Co. Ltd Germany) at a wavelength of 540 nm, and the 134 calculation formula for the hemolysis rate is eqn. 5: Hemolysis ratio (%)= $(A_s-A_n)/(A_p-A_n)\times100$ , 135 where  $A_s$  is the absorbance of the tested sample suspension.  $A_n$  and  $A_p$  were regarded as the 136 absorbance of the negative control and the positive control, respectively.

137 In vivo studies

Wistar adult female rat (180 g, 12-14 weeks old) were purchased from Benxi Longevity Biology 138 139 (Benxi, China), and the animals were housed in cages at 25 °C, and fed with standard pellets and water ad libitum. An incision of length 2 cm was made in the dermal skin of the rat's back near the 140 141 neck (wiped with 70% alcohol). Rats were anesthetized using thiopental sodium (dose of 25 mg per kilogram of body weight) for all surgical procedures.<sup>[8]</sup> The animals were randomly divided into 142 two groups: the animals in group I (n=2) were sutured with traditional sutures, and the obtained 143 144 SMP sutures were used to suture the animals in group II (n=4). The obtained SMPs were made into 0.5 mm width and 0.2 mm thickness and autoclaved before the suturing experiment. Note: animal 145 146 experiments were performed according to the Guidelines of the Liaoning Administrative Committee 147 on Animal Research.



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**S**7

- 151 (G", dotted line) of the  $P_3$  vs. frequency at room temperature; (b) The G' and G" of the  $P_3$  vs.
- 152 temperature at a fixed frequency of 1 Hz.



153

154 Fig. S2 the self-healing behavior of the obtained SMPs with an almost fully healing within 130 min

155 at 37 °C or 10 min at 50 °C.

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158 Fig. S3 The the mechanical strengths changed of the obtained P<sub>3</sub> after 8 days of degradation



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160 Fig. S4. H&E stained cross-sections of the self-healing of SMPs suture site skin of two groups on

161 the 5 th days after the surgery.

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