## Supplementary information Viscoelastic microfluidics for enhanced separation resolution of submicron particles and extracellular vesicles

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Fig. S1. CAD design of the co-flow microfluidic device.



**Fig S2**. Time-lapse images of the flow oscillation in 5,000 ppm PEO concentration for 100 nm particles (pseudo-coloured red) at the cross junction of the microfluidic device. (a) The particles from the side channels flow into the main straight channel at t = 0.4 s. (b)-(e) Gradually sheath flow from the middle becomes dominant and pushes the particle flow towards the inlet from t = 1.6 s to t = 2.4 s. (f) Particles are completely pushed beyond the boundary of the microscopic focusing area at t = 2.8 s. (g)-(i) Sample flow overcomes the resistance of the sheath flow and gradually flows towards the straight section of the microfluidic device through the coss junction from t = 4.6 s to t = 6 s. (j) The particles from the side channels flow into the main straight channel as usual at t = 6.8 s.



**Fig. S3**(A) Fluorescent trajectories of 50-nm (pseudo-coloured red) polystyrene particles at the expansion region of the co-flow microfluidic device under different PEO concentrations. When increasing the PEO concentration to 3,000 ppm or above, we observed 50-nm particles migrated from the channel side walls toward the channel centre. Due to the flow oscillations at PEO concentrations of 3,000 ppm and 5,000 ppm, we used a flow rate ratio of 4:1 for those PEO concentrations to ensure the flow is stable. (B) Normalised fluorescence intensity of particle distribution across the yellow dotted line.



**Fig. S4.** CAD design of the sheathless microfluidic device used for high concentration PEO concentration experiments to investigate the focusing of nanoparticles.



**Fig. S5.** Fluorescent trajectories of 100-nm (pseudo-coloured red), 200-nm (pseudo-coloured yellow) and 500-nm (pseudo-coloured green) polystyrene particles at the expansion region of the sheathless microfluidic device for 5,000 ppm PEO aqueous solution.



Fig. S6. Design of a parallelised microfluidic device with straight channels to enhance the throughput.

Separation mechanism	Particle sizes	Separation resolution	Biological particles	Separation purity	Separation efficiency	Throughput	References
Ultracentrifugation	50–200 nm	100-150 nm	Exosomes, EVs	N/A	23% - 70%	53 μL/min	1–3
Ultrafiltration	50-250 nm	150 nm	Exosomes, natural organic matters	91.5%	70% - 82%	16 mL/min	46
Size exclusion chromatography	50–200 nm	120-150 nm	Exosomes	N/A	80%-90%	0.5 mL/min	7–9
Acoustophoresis	100–900 nm	230 nm	EVs	98%	> 90%	4- 80 μL/min	10
Electrophoresis	100-1,000 nm	400 nm	Exosomes	N/A	65% - 98%	$1 \mu L/min$	11
Magnetophoresis	5 nm-200 nm	800 nm	EVs	80%	80% - 90%	2.5 µL/min	12
Inertial microfluidics	200 nm–2 µm	800 nm	EVs	N/A	15% - 97%	80 µL/min	13,14
Deterministic lateral displacement	51 nm-1.5 μm	150 nm	EVs	98%	39%	0.05 μL/ min	15,16
Microfluidic filtration	30–200 nm	150 nm	Exosomes	N/A	74%	40 µL/min	17
Pinched flow fractionation	30 nm–2 μm	400 nm	EVs	N/A	70% - 90%	20 µL/min	18
Viscoelastic microfluidics	100 nm– 2 μm	400 nm	Exosomes, EVs	96%	93%	3 µL/min	19,20
Viscoelastic microfluidics	100–500 nm	100 nm	EVs	40% - 90 %	50% - 86%	3 μL/min	This study

Table S1	Summary	of submicron	and nanopa	rticle separation	techniques
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