

1            ***Electronic Supplementary Information (ESI) for***  
2            **Smart Zwitterionic Coatings with Precise pH-Responsive**  
3            **Antibacterial Functions for Bone Implants to Combat**  
4            **Bacterial Infections**

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19   This supporting information includes:

20   (1) Methods: 1 to 10

21   (2) Supplementary Figures: Figure. S1 to S5.

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## 23 **Methods:**

### 24 **1 characterization of the PSB/GS-loaded coating onto the Titanium Surface**

25 The surface morphology as well as the elemental compositions of pristine titanium,  
26 PSB coating and PSB/GS coating were investigated using a Scanning electron  
27 microscopy. X-ray photoelectron spectroscopy was performed using a monochromatic  
28 Al K $\alpha$  (1486.6 eV) X-ray source. Since the macroscopic shape of the titanium foils were  
29 found to be too irregular for determining the coating thickness and surface wettability,  
30 regular shaped (1  $\times$  1 cm) monocrystalline silicon wafers were used to deposit PSB  
31 coating and PSB/GS coating instead of titanium foils. The changes in surface  
32 wettability of PSB and PSB/GS coatings were investigated using an OCA20 contact  
33 angle measurement device. The thickness of the PSB coating and PSB/GS coating were  
34 then examined by a spectroscopic ellipsometer.

### 35 **2 Drug-release behavior of PSB/GS coating**

36 The PSB/GS coating was placed in a well plate and PBS solutions of different pH  
37 (pH 7.4; pH 5.5) were added dropwise. At regular intervals, 500  $\mu$ L of drug release  
38 solution was removed from the well plates and 500  $\mu$ L of PBS solution at pH 7.4 or 5.5  
39 was added. Subsequently, the establishment of the standard curve required the use of a  
40 UV-visible spectrophotometer to determine the concentration of GS and the use of  
41 acetyl acetone–formaldehyde as a derivatizing reagent and boric acid–acetic acid as a  
42 buffer. Following this, the cumulative release curve of GS over a 30-day period was  
43 calculated.

### 44 **3 Zone of inhibition assay**

45 Bacterial suspensions ( $10^5$  CFU mL<sup>-1</sup>) were added to agar medium, mixed well and  
46 spread flat in Petri dishes. The two samples (PSB coating and PSB/GS coating) were  
47 carefully placed in the center of the petri dish and the dish was incubated at 37°C for  
48 24 h. The diameter of the zone of inhibition was recorded.

#### 49 **4 Bacterial anti-adhesion ability**

50 The bacterial suspension ( $2 \times 10^8$  CFU mL<sup>-1</sup>) was co-cultured with the pristine Ti,  
51 PSB coating, and PSB/GS coating for 24 h, and then the pristine titanium, PSB coatings,  
52 and PSB/GS coatings were rinsed with PBS to remove loose bacteria. The samples were  
53 then immersed in PBS and sonicated, which was repeated 5 times. After staining, the  
54 bacterial status of the sample surface was observed by CLSM. In addition, after diluting  
55 to the appropriate concentration, the bacteria were cultured onto the NA plates and  
56 incubated for 24 h. the bacterial antiadhesion rate was calculated using a plate counting  
57 method as following formula:

$$\begin{aligned} & \text{Bactericidal anti - adhesion rate (\%)} \\ & = \frac{\text{cell count of control} - \text{cell count of samples}}{\text{cell count of control}} \times 100\% \end{aligned}$$

58

#### 59 **5 Antibacterial assay**

60 Sterilized pristine Ti, PSB coating and PSB/GS coating were placed into 12-well  
61 culture plates, and 100 μL of bacterial suspension ( $10^5$  CFU mL<sup>-1</sup>) was added to each  
62 well. The samples were incubated at 37°C for 24 h at a humidity of not less than 90%,  
63 then removed, washed with 5 mL of PBS, and the solution was diluted 10-fold. Finally,  
64 20 μL of the diluted solution was spread on the plate and incubated at 37°C for 24 h.  
65 The number of bacterial colonies on the plate was recorded and the antibacterial rate  
66 was calculated according to the following formula:

$$\text{Antibacterial rate (\%)} = \frac{CFU \cdot mL^{-1}_{0h} - CFU \cdot mL^{-1}_{24h}}{CFU \cdot mL^{-1}_{0h}} \times 100 \%$$

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68 where CFU represents the number of colonies counted per plate at the indicated times,

69 and bactericidal rate is taken as the average of the data from six parallel samples.

## 70 **6 Antibiofilm assay**

71 Pristine Ti, PSB coating and PSB/GS coating were immersed in a bacterial

72 suspension at a concentration of  $10^7$  CFU mL<sup>-1</sup> and incubated at 37°C for 24 h before

73 the samples were removed and rinsed three times with PBS. This process was repeated

74 daily for 7 days. Finally, images of pristine titanium, GS-coated and PSB/GS-coated

75 titanium foils were observed by scanning electron microscopy (SEM). Biofilm biomass

76 and bacterial counts on the samples surface were measured using crystal violet staining

77 and well plate counting methods, respectively.

## 78 **7 Hemocompatibility**

79 After centrifugation (1300 rpm, 10 min) of fresh anticoagulated rabbit blood, 1.2 mL

80 of red blood cells from the bottom of the centrifuge tube is diluted to 50 mL (2.4 v/v%)

81 with saline. Pristine Ti and PSB/GS coating were submerged in diluted erythrocyte

82 solution to detect hemolysis. The red blood cell suspensions treated with deionized

83 water and saline were used as positive and negative controls, respectively. All samples

84 were shaken at 37°C for 1 h and then centrifuged (8000 rpm, 5 min). The supernatants

85 after centrifugation were taken and the absorbance of hemoglobin was measured at 540

86 nm with a spectrophotometer (UV-2700, Shimadzu instruments). The hemolysis ratio

87 of the sample was calculated using the following formula:

88 
$$\text{Hemolysis ratio (\%)} = \frac{A_{\text{Sample}} - A_{\text{Negative control}}}{A_{\text{Positive control}} - A_{\text{Negative control}}} \times 100 \%$$

## 89 **8 Biocompatibility**

90 To evaluate the biocompatibility of the pristine Ti and PSB/GS coating *in vitro*, the  
91 toxicity of the sample extracts to L929 cells was assessed using the CCK-8 method, and  
92 PBS was served as the control. L929 cells were inoculated into 96-well plates and  
93 incubated for 24 h (37°C, 5% CO<sub>2</sub>). The cell culture medium was then replaced with  
94 the sample extract for another 24 h of incubation. At last, CCK-8 reagents were added  
95 to the 96-well plates and their absorbance at 450 nm was detected using a microplate  
96 reader. The morphology of L929 cells was observed using fluorescent staining.

## 97 **9 In vivo host response**

98 Before the experiment, the samples (5 × 5 mm) were sterilized by UV irradiation for  
99 a period of 2 h. Next, the samples were implanted into the skin of the dorsal surface of  
100 the mice and the relevant areas were labeled. At days 3 and 7 of sample implantation,  
101 the marked skin was picked up with forceps and the skin tissue surrounding the center  
102 point that was in touch with the sample was cut with sterile surgical scissors. The  
103 sampled skin tissues were fixed using 4 % paraformaldehyde. Finally, H&E staining  
104 was performed for microscopic examination and picture collection for analysis.

## 105 **10 Antifouling assay**

106 Bovine serum albumin (FITC-BSA) was diluted to 0.1 mg/ml in PBS, and the  
107 prepared layer samples were immersed in the protein solution and incubated under dark  
108 conditions at 37°C for 1 h. The sample surface was washed with PBS solution to remove  
109 non-adhered proteins on the surface, and the procedure was repeated three times. The

110 protein adhesion on the sample surface was then observed using confocal laser scanning  
111 microscope and the expression was quantified by relative fluorescence intensity.

### 112 **11 Blood adhesion assay**

113 Hematocrit adhesion test was performed according to a previously reported study.  
114 Fresh rabbit blood was separated into platelet-rich plasma and RBCs suspensions by  
115 centrifugation at 1500 rpm for 15 min. The prepared samples were then co-cultured  
116 with platelets and RBCs and incubated at 37°C for 1 h. At the end of the incubation,  
117 saline rinses were used at least three times to remove non-adhered blood cells. The  
118 samples were fixed using 2.5 wt% glutaraldehyde, followed by gradient dehydration of  
119 the samples using ethanol. SEM was then used for observation. Quantitative expression  
120 of adhesion was performed.

### 121 **12 *Ex vivo* antithrombogenicity assay**

122 An arteriovenous shunt model was established in three adult New Zealand rabbits  
123 (2.5 kg ~ 3 kg) for an *in vitro* antithrombotic test. First, anesthesia was performed, and  
124 then the carotid artery and external vein were separated to establish the *in vitro* circuit.  
125 The prepared coated samples were assembled with the *in vitro* circuit, and after blood  
126 circulation for 2h, the samples were collected and simply washed with saline.  
127 Photographs were taken to record cross-sectional and surface images of thrombus  
128 formation. Thrombus weight and duct closure rate were quantitatively expressed. In  
129 addition, the internal morphology was observed by SEM.

### 130 **13 *In vivo* antibacterial assay in a rat model**

131 The rats were anesthetized intraperitoneally, and a 2 cm long skin incision was made

132 on the back of the rats to create a subcutaneous pocket. Two animal models were  
133 established in this work. For the first one, 30  $\mu\text{L}$  of *S. aureus* suspension ( $10^8$  CFU  
134  $\text{mL}^{-1}$ ) was first injected into the implantation area, and 30 min later the Ti samples were  
135 implanted and the incisions were sutured. For the second one, the implanted Ti samples  
136 were first immersed in *S. aureus* solution ( $10^9$  CFU  $\text{mL}^{-1}$ ) for 30 min, and then the  
137 samples were continued to be implanted and sutured as mentioned above. In each of  
138 these two models, six rats were used in each parallel group. The Titanium foils were  
139 kept for 3 days after implantation, and then the SD rats were sacrificed. The implanted  
140 Titanium foils and the surrounding subcutaneous tissue were removed from the  
141 corresponding areas. In order to observe the colonization of bacteria on the surface of  
142 the implanted Titanium foils, CLSM was used to observe the bacteria on the surface of  
143 the implanted Titanium foils, meanwhile, plate counting method was used for  
144 quantitative counting. In addition, CD68 antibody and CD3 antibody were used to label  
145 macrophages cells and T lymphocytes, respectively.

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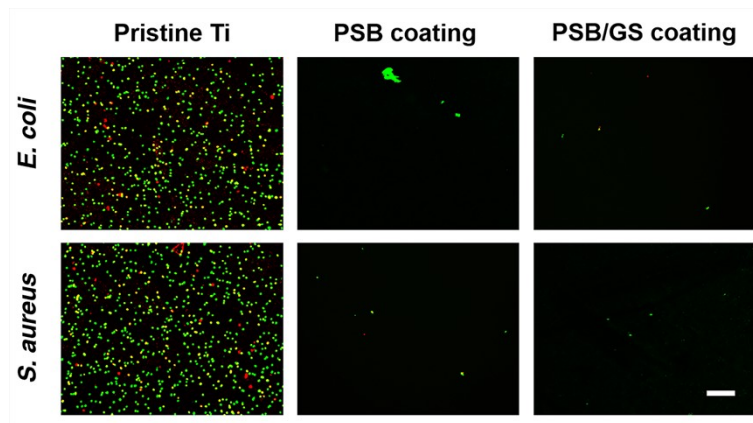
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154 **Figures:**

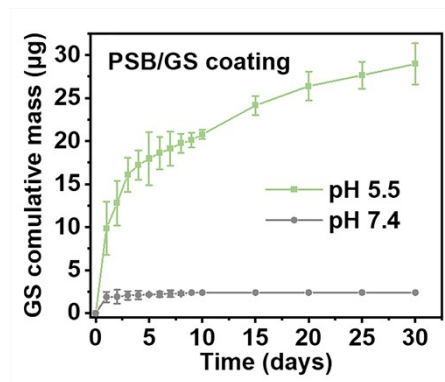


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156 **Figure. S1** Fluorescence microscopic images of Live/Dead labeled bacteria showing  
157 adhesion on the surface of pristine Ti, PSB coating and PSB/GS coating. Scale bar: 20

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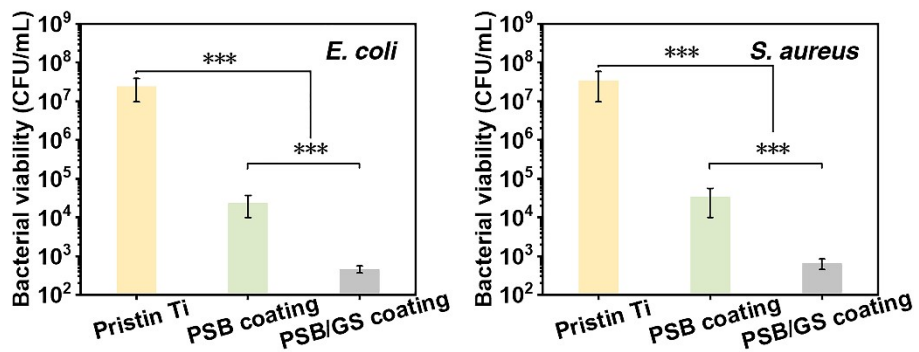
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**Figure. S2** GS cumulative release mass of the PSB/GS coating.



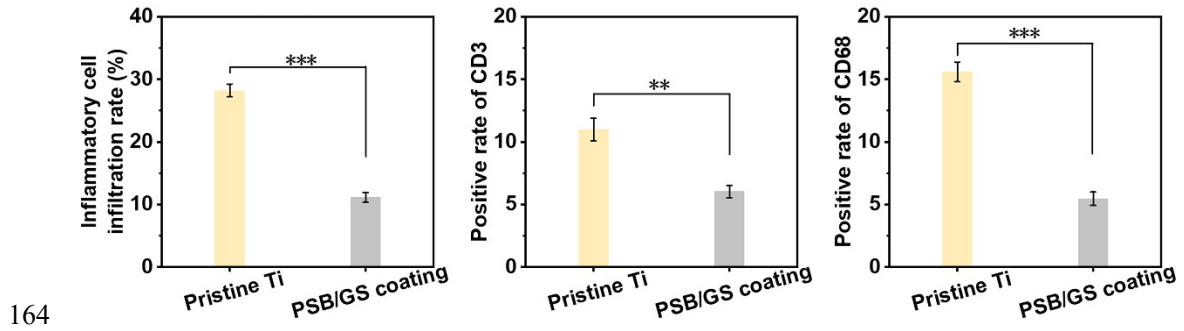
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162 **Figure. S3** The bacterial number on the pristine Ti, PSB coating and PSB/GS coating

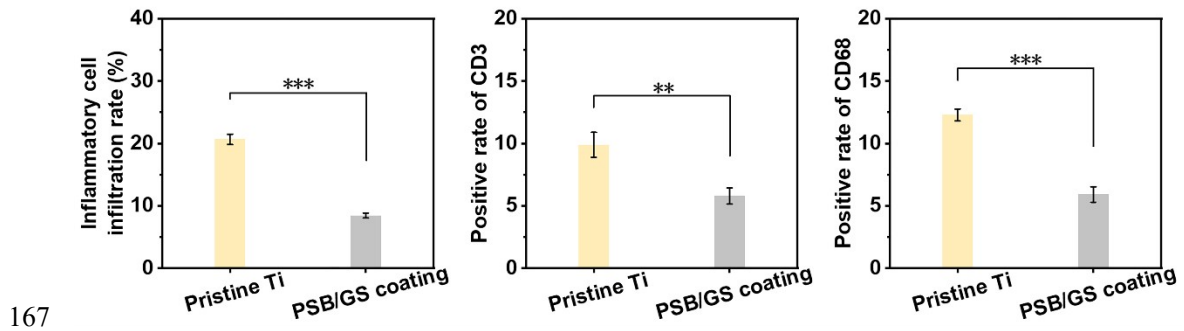
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after 7 days.





165 **Figure. S4** *On vitro* model of infection, quantitative analysis of the H&E-, CD68-,  
 166 and CD3-stained tissues surrounding the sample 3 days after implantation.



168 **Figure. S5** *On vivo* model of infection, quantitative analysis of the H&E-, CD68-, and  
 169 CD3-stained tissues surrounding the sample 3 days after implantation.