1	Supplementary Information for
2	
3	Metainterface with mechanical, thermal, and active programming based on
4	programmable orientation-distributed biometric architectonics
5	
6	Zhenyang Gao ^{1,2} , Hongze Wang ^{1,2,3,4*} , Pengyuan Ren ^{1,2} , Gengchen Zheng ^{1,2} , Yang
7	Lu ⁵ , Bokang Peng ^{1,2} , Zijue Tang ^{1,2} , Yi Wu ^{1,2,3*} , Haowei Wang ^{1,2,3}
8	
9	¹ State Key Labortory of Metal Matrix Composites, Shanghai Jiao Tong University,
10	Shanghai, 200240, China.
11	² School of Materials Science and Engineering, Shanghai Jiao Tong University,
12	Shanghai, 200240, China.
13	³ Institute of Alumics Materials, Shanghai Jiao Tong University (Anhui), Huaibei,
14	235000, China.
15	⁴ Shanghai Key Laboratory of Material Laser Processing and Modification, Shanghai,
16	200240, China.
17	⁵ Department of Mechanical Engineering, the University of Hong Kong, Hong Kong,
18	999077, China.
19	*Corresponding authors. E-mail: hz.wang@sjtu.edu.cn, eagle51@sjtu.edu.cn
20	
21	
22	This PDF file includes:
23	Supplementary Notes 1 to 3
24	Figures S1 to S30
25	Tables S1 to S7
26	Captions for Movies S1 to S7
27	
28	Other supporting materials for this manuscript include the following:
29	Movies S1 to S7

30 Supplementary Note 1. Design rationales, advantages, and crack extension

31 mechanisms for metainterface.

Programming the interface properties requires highly anisotropic behaviors of the interface design unit. In comparison to various sharp edges found in biological structures ^{1, 2, 3} (Figure S1), honeybee stinger has evolved with highly anisotropic geometries, characterized by their backward barbs, rendering it an ideal choice for designing interface elements with programmable anisotropic mechanical and dynamical properties ^{4, 5, 6}. Those stingers have three-dimensional features with limited sizes ranging from micro- to nanoscales⁷, making them difficult to observe, reconstruct, and manufacture.

40 To interpret the underlying mechanisms responsibly for the mechanical advantages of the metainterface featuring XCT-rebuild biostructures in comparison to 41 42 interfaces with highly simplified biometric geometries, we quantified crack extensions 43 mechanisms (theoretical diagram in Figure S27 (a)) from the substrate to the interface 44 design area using the ZEISS Xradia 520 Versa X-ray microscopic equipment, offering 45 a resolution of 29.203 µm (Figure S27 (b-d) and Supplementary movies Movie S1, also 46 consult Figure S19 and Section 4.5 in Methods for additional details). In contrast to the 47 interfaces with the simplified biometric geometries, it is evident that a greater number 48 of microcracks extend from the substrate to the XCT-rebuild stingers. This mechanism 49 underscores the enhanced effectiveness of XCT-rebuild biostructures in leveraging the 50 rigid interface surface to redistribute mechanical stress and fracture energies during 51 interfacial decoupling, substantiating the mechanical advancements brought about by 52 the XCT-rebuild geometries in this study. The fracture process of the metainterface is simulated using finite element analysis (FEA) as shown in Figure S28. The simulation 53 54 reveals that the XCT-reconstructed stinger geometry initiates microcracks, which 55 gradually extend to form a major crack leading to complete fracture. This 56 microcracking mechanism allows significant stress distribution to the substrate surrounding the stinger geometry, enhancing the mechanical modulus, strength, and 57 58 absorbed interfacial energy during the interface decoupling process. In addition, we assessed the designability of different interfaces in Figure S29. Existing designs (Figure 59 60 S29 (a-b)) often feature simple empirical or bioinspired geometries with limited control 61 over interface anisotropic properties in a single direction. In contrast, the metainterface 62 (Figure S29 (c)) consists of a minimum design unit, the single stinger, which orients 63 itself to provide highly programmable and localized thermomechanical behaviors that 64 were previously unattainable.

65 Supplementary Note 2. Effects of metainterfaces on composite metamaterials with

66 bending-dominated and stretch-dominated lattice implants.

67 In bending-dominated composite metamaterials, there is a 3% (vintiles) to 11% (SHS) 68 improvement in SEAs compared to their conventional counterparts, while stretch-69 dominated metamaterials exhibit a 9% (BCC) to 18% (FCC) improvement in SEAs, as shown in Figure 3 (c). Stretch-dominated lattices display higher stress-strain curves 70 71 compared to bending-dominated structures, and the improvements in SEAs facilitated by metainterfaces are more pronounced. For example, the results of struct-based lattice 72 73 topologies indicate that the SEA improvements in stretch-dominated lattices are 3 to 9 74 times higher than in bending-dominated lattices. In addition, an increase in the interface area introduces greater improvements in SEAs, as seen in the case of SHS filled with 75 metainterfaces, which exhibit a 4-fold improvement in SEAs compared to vintiles. 76 77 These results provide valuable design guidelines, suggesting that metainterfaces

78 with stiffer interface parent geometries and a larger interface contact area yield more 79 significant mechanical advancements. Furthermore, it is evident that the truss elements of bending-dominated composite metamaterials (Figure S25) tend to fracture 80 81 prematurely compared to the stretch-dominated lattices (Figure 4 (e)). This premature 82 fracture results in an early separation of the matrix and reduced interface reactions, 83 which in turn explains the observed early decline in the stress-strain curves in Figure 84 S24 and the less pronounced improvements in SEAs in bending-dominated structures. 85 Moreover, the occurrence of interfacial fractures underscores the findings that 86 increasing the contact interface area equipped with metainterfaces leads to more 87 effective enhancements in both SEAs and stress-strain curves. In addition, it is observed 88 that the truss of the bending-dominated composite metamaterials exhibit an early 89 fracture compared to the stretch-dominated lattices, leading to an early separation of 90 the matrix and lower interface reactions. This explains the observed earlier decay of the 91 stress-strain curves, and less effective improvements in SEAs of bending-dominated 92 structures.

Supplementary Note 3. Case studies of active programming in amphibious robotic feet To demonstrate the versatility of the metadisk, we have explored its potential application in amphibious robotic feet (Figure S26 (a)), which can exhibit programmable mechanical behaviors on land using the design principles described in equations (6-8), and achieve programmable flow control in water. By precisely controlling the concentration angle, this robotic foot can effectively concentrate and direct the flow to desired locations Figure S26 (b-c), achieving flow modulation ranging from 96% to 115% of the inlet flows as the concentrating angles vary from 0° to 60° (Figure S26 (d)). This illustrates the potential of employing metainterfaces in systems with programmable multifunctionalities, such as real-time controlled mechanical interface reactions and flow controls. 104 Supplementary figures and tables105



- 106
- 107 Figure S1. The sharp geometries of different species with increasing anisotropy
- 108 including the teeth from leech ¹, the teeth from dogfish ², stinger from wasp ³, stinger
- 109 from mosquito 2 , and stinger with backward barbs from honeybee 8 .



110Programmable amphibious finsProgrammable biometric roset111Figure S2. Potential applications of metadisk in various robotics systems.



113 Figure S3. Experimental designs and testing of flexible 80A specimen directly cured

114 from liquid. (a) Specimen preparation. (b) Results of the mechanical testing.



- 117 Figure S4. Designs and shear and tensile experiments for the measurement of coupled
- 118 interface energies. (a) Design and preparation of specimens. (b) Experimental process.





120 121 Figure S5. Stress-strain curves of the metainterfaces and interfaces without stingers

122 under coupled stress condition.





125 Figure S6. Designs and shear experiments for the measurement of uncoupled interface

126 energies. (a) Design and preparation of specimens; and (b) Experimental process.







stingers under compression.





134 under uncoupled stress condition.



136 Figure S9. (a) The printed stingers with sizes ranging from 500 to 2000 μ m. (b-d)The 137 surface finishes captured by Zeiss AX10 optical microscope for the with 250 μ m

138 stingers, 500 µm stingers, 1000 µm stingers, respectively.







- 142 by the modulus of the parent material for the thermos-mechanical metamaterial and its
- 143 conventional counterpart designed in this work.

Training data generation



145146 Figure S11. Flowcharts of machine learning process.



148

149 Figure S12. Configurations for thermodynamical simulations. (a) The computational 150 domain and boundary condition of the simulation. (b) Different outlet faces of the

151 simulation. (c) The training data slices for flow rate image processing algorithm. (d)

152 The training data slices for heat exchange rate image processing algorithm.



154 155 Figure S13. Training data distribution. (a) The heat exchange rate outputs with different

156 training inputs. (b) The velocity outputs with different training inputs.



158 159 Figure S14. Prediction test errors reduces as the number of training data increases for

160 predicting (a) velocity, and (b) temperature.





162 Figure S15. Prediction test errors for differrent hyperparameters of the FCNNs to

163 predict (a) velocity, and (b) temperature.



predicting (a) velocity and (b) temperature.



169

Figure S17. The thermodynamical programming algorithms. (a) Theoretical flow rate 170 and heat exchange rate design schematics and (b) flow charts of programming the flow 171 rate and heat exchange rate. Note that $\theta_{s,X}$ represents the stinger angle of the stinger X, v_{X-Y} is the flow rate from stinger X to stinger Y, θ_{X-Y} represents the angle between the 172 173 velocity v_{X-Y} and stinger Y, ΔT_{R1-R2} represents the temperature difference between the 174 regions R^1 and R^2 , n is the batch size of the RGM-modified deep search algorithm, 175 $v_{surrounding}$ is the negative flow contribution caused by the surrounding structures of the 176 metamaterials, A_{cell} represents the area of a unit cells implanted with four stingers, 177 ΔQ_{top} and ΔQ_{side} represent the total heat exchanged from the top flows and the side flows, 178 respectively, v_{top} and v_{side} are the outlet flow rates from the top flows and the side flows, 179 respectively, q and v represent the desired heat exchange rate and the outlet velocity, 180 181 respectively.



183 Figure S18. The simulation configuration to calculate the interface stresses of 184 metainterfaces and interfaces without stingers. (a) Uncoupled stress conditions. (b) 185 Coupled stress conditions. (c) The definition of the interface depth and the 186 corresponding plane for interface stress average calculations.



- Figure S19. The XCT experiments. (a) Flow chart of XCT experiments using the BL18B beamline of Shanghai Synchrotron Radiation Facility (SSRF). (b) Flow chart
- 191 of XCT experiments using the ZEISS Xradia 520 Versa X-ray microscope at 192 Instrumental Analysis Center of Shanghai Jiao Tong University (SJTU).



- 193 194 Figure S20. The re-construction of stinger geometries based on the XCT results on a
- 195 freeform geometry.



Figure S21. XCT images of internal interface fractures. (a) Spherical hollow structures (SHS) metamaterials with metainterfaces. (b) SHS metamaterials with conventional interfaces. (c) Body-centered-cubic (BCC) metamaterials with metainterfaces. (d) BCC metamaterials with conventional interfaces. (e) Tesseract metamaterials with conventional interfaces. (F) Tesseract metamaterials with conventional interfaces.



204

205 Figure S22. Interface modifications included in this study. (a1-a5) The conventional 206 interface modifications with rectangular shapes. (b1-b5) The conventional interface 207 modifications with wavy shapes. (c1-c5) The conventional interface modifications with 208 traingular shapes. (d1-d5) The biometric interface modifications inspired by stinger from honeybee. (e1-e5) The biometric interface modifications inspired by stinger from 209 210 parasite. (f1-f5) The trapezium biometric interface modifications inspired by elytra of 211 beetle. (g1-g3) The ellipse biometric interface modifications inspired by elytra of 212 beetle. (h) The metainterface designed with XCT-rebuild stinger geometry of 213 honeybee.



214 E_t/E_0 215 Figure S23. Ashby chart comparing the Tensile strength σ_t and tensile modulus E_s for 216 different interfaces normalized by the modulus of parent material E_0 of metainterfaces 217 and existing interface designs including the flat interface, interface modified by 218 empirical conventional rectangular, traingular, and wave shapes ⁹, inspired by stingers 219 of honeybee ¹⁰ and parasite ¹¹, and elytra of beetle with trapezium ¹² or ellipse ¹³ 220 simplifications. Note that the pentagon represents the metainterface with highest tensile 221 strength and modulus.



Figure S24. The normalized compressive stress-strain curves of pure lattice structures

224 fabricated with clear V4 resin, pure matrix materials prepared with flexible 80A resin, 225 composite metamaterials with and without programmed metainterfaces.



227 Figure S25. The interface cracks for bending-dominated vintiles composite 228 metamaterials with and without programmed metainterfaces.



230 231 Figure S26. (a) Amphibious robot feet with programmable uncoupled mechanical and 232 thermodynamical behaviors, where the inlet flow rate is set to 4 m/s, θ_c is the flow 233 concentrating angle. (b-c) Flow velocity distributions at y and x direction, respectively, 234 of the amphibious robot feet with $\theta_c = 0^\circ$ and $\theta_c = 60^\circ$. (d) Programmable concentrated 235 flow velocity for different θ_c .



236 237 Figure S27. The (a) theoretical crack distribution diagram and XCT-scanned crack

238 extensions from the substrate to the interface design regions for (b) metainterface with

239 XCT-rebuild biostructure, (c) interface inspired by honeybee-stinger, and (d) interface 240 inspired by elytra of beetle.



242 243 Figure S28. Simulated fracture process of metainterface under (a) shear and (b) tensile 244 load conditions.



- 246 247
- 248 Figure S29. Schematic diagrams of the interface directional designability for (a)
- 249 interfaces with conventional modifications or inspired by elytra of beetle, (b) interfaces 250 inspired by stinger of honeybee, and (c) metainterfaces.



251252 Figure S30. Fabricated freeform metainterface.

Table S1. The post-processing conditions of the parent materials for different types ofexperiment.

Experiment	Initial form	Curing time (minutes)	Curing temperature (°C)
Basic mechanical properties of parent materials (standard clear)	Printed solids	15	60
Basic mechanical properties of parent materials (flexible 80A)	Printed solids or liquid	2.5-12	60
Metainterfaces and conventional interfaces for the measurement of coupled interface energy (standard clear)	Printed solids	5	60
Metainterfaces and conventional interfaces for the measurement of uncoupled interface energy (standard clear)	Printed solids	15	60
Substrates of metainterface for the measurement of coupled interface energy (flexible 80A)	Printed solids with adhered liquid	10	60
Substrates of metainterface for the measurement of uncoupled interface energy (flexible 80A)	Printed solids	10	60
Vertical stress measurement (standard clear)	Printed solids	15	60
Vertical stress measurement (flexible 80A)	Printed solids	10	60
Metainterfaces and conventional interfaces of composite metamaterials (standard clear)	Printed solids	3	60
Metainterfaces and conventional interfaces of composite metastructures (standard clear)	Printed solids	15	60
Substrates of composite metamaterials (flexible 80A)	Liquid	12	60
Substrates of composite metastructures (flexible 80A)	Printed solids	10	60

Table 52. Weenamear properties of parent materials.					
Specimen type	Modulus (MPa)	Ultimate tensile stress (MPa)	Fracture strain (%)		
Specimen 1 (flexible 80A)	4.45	3.80	85.49		
Specimen 2 (flexible 80A)	4.41	3.76	87.07		
Specimen 3 (flexible 80A)	4.47	3.81	84.93		
Specimens (liquid cured flexible 80A)	3.13 - 4.39	1.66 - 3.79	53.80 - 86.75		
Specimen 1 (standard clear)	1662.52	48.97	8.36		
Specimen 2 (standard clear)	1655.43	46.35	9.15		
Specimen 3 (standard clear)	1669.34	50.23	7.97		

257 Table S2. Mechanical properties of parent materials.

Topology	Diameter or thickness of samples (mm)	Interface type	Struct diameter (mm)	Relative density (%)	Assembly type	Weight (g)	
		Without metainterface	1.00		With flexible matrix	13.51	
	_			6.44	Without flexible matrix	0.87	
BCC	2	XX 7'.1			With flexible matrix	13.45	
		With metainterface	0.84	6.62	Without flexible matrix	0.89	
		W/d			With flexible matrix	13.38	
ECC	2	metainterface	1.00	9.57	Without flexible matrix	1.28	
FCC	2	With		9.53	With flexible matrix	13.74	
		With metainterface	0.91		Without flexible matrix	1.31	
		Without metainterface	1.00	4.33	With flexible matrix	13.62	
					Without flexible matrix	0.59	
SHS	1	With metainterface	0.85	4.24	With flexible matrix	13.43	
					Without flexible matrix	0.57	
		Without metainterface	1.00		With flexible matrix	13.44	
				4.17	Without flexible matrix	0.56	
Vintiles	2	With			With flexible matrix	13.34	
		With metainterface	0.93	4.42	Without flexible matrix	0.59	
		W/d			With flexible matrix	13.70	
T		metainterface	1.00	7.01	Without flexible matrix	0.96	
Iesseract	2	XX7*41			With flexible matrix	13.10	
			With metainterface	0.88	7.10	Without flexible matrix	0.93
NA	NA	NA	NA	NA	Pure matrix	13.47	

259 Table S3. Summary of weights for the components of composite metamaterials.

Type of composite metastructures	Thickness design of each rigid sheet (mm)	Average weight of each rigid sheet (g)	Thickness design of flexible matrix between the sheets (mm)	Average weight of flexible matrix (g)	Density (g/cm ³)	Sheet-to- matrix volume ratio (%)
Composite metastructure without metainterfaces	1	0.49	3.5	13.65	1.1	3.6
Composite metastructure with metainterfaces	0.5	0.51	4	13.58	1.1	3.7

261 Table S4. Summary of weights for the components of composite metastructures.

263 Table S5. Summary of design information and relative densities for the thermos-

1	mashaniaal matamatanial	and its convention	al against am ant degion	ad in this month	
4	mechanical metamaterial and its conventional counterpart designed in this work.				
	Ture of motomotorials	Beam diameter	Average relative	Average normalized	
	Type of metamaterials	(mm)	densities (%)	modulus (MPa/MPa)	
	Thermos-mechanical metamaterials	0.416	20.7	0.18	

20.7

0.17

	2	0		
264	mechanical metamaterial	l and its conventiona	al counterpart desig	ned in this v

0.5

265

Conventional

metamaterials

Turne of ECNIN	FCNN for velocity	FCNN for temperature			
Type of Fernin	prediction	prediction			
Number of hidden layers	2	2			
Number of neurons per layer	50	30			
Training epochs	2000	2500			
Activation function	ReLU	ReLU			

266 Table S6. The hyperparameters used in FCNNs.

50	¹ <u>rable 57. The design parameters of the interfaces used in this study.</u>			
	Interface design	Parameter type	Parameter range	
	Programmable metainterface with XCT-rebuild biostructure	Stinger angle	0 to 180 degrees	
	Interface inspired by elytra of beetle (ellipse)	Blade angle	15 to 40 degrees	
	Interface inspired by elytra of beetle (trapezium)	Tooth width	0.5 to 2.5 mm	
	Interface inspired by stinger of parasite	Stinger densities	0.64 to 1.44 mm ⁻²	
	Interface inspired by stinger of honeybee	Bending curvature	1 to 2.5 mm ⁻¹	
	Interface modified by rectangular geometry	Size of the rectangle	0.5 to 2.5 mm	
	Interface modified by triangular geometry	Size of triangular base	0.5 to 2.5 mm	
	Interface modified by wavey geometry	Size of wave periods	1 to 5 mm	

268 Table S7. The design parameters of the interfaces used in this study.

270 Captions for supplementary movies

- 271 Movie S1 (separate file). Comparison of internal fractures between metainterface with
- 272 XCT-rebuild biostructures and biometric interfaces.
- 273 Movie S2 (separate file). Comparison of internal fractures for face-centered-cubic
- 274 (FCC) metamaterials.
- 275 Movie S3 (separate file). Comparison of internal fractures for BCC metamaterials.
- 276 Movie S4 (separate file). Comparison of internal fractures for tesseract metamaterials.
- 277 Movie S5 (separate file). Comparison of internal fractures for SHS metamaterials.
- 278 Movie S6 (separate file). Comparison of internal fractures for vintiles metamaterials.
- 279 Movie S7 (separate file). Motion and programmed interface mechanics of robotics
- 280 exoskeleton.

281 References

- H. Ayhan, N. Özyurt Koçakoğlu and S. Candan, *Microscopy Research and Technique*, 2021, 84, 2930-2935.
- 284 2. M. Meyers, A. Lin, Y. Lin, E. Olevsky and S. Georgalis, *Jom*, 2008, 60, 19-24.
- 285 3. Z.-L. Zhao, H.-P. Zhao, G.-J. Ma, C.-W. Wu, K. Yang and X.-Q. Feng, *Biology* 286 open, 2015, 4, 921-928.
- 287 4. Y. Lu, T. Ren, H. Zhang, Q. Jin, L. Shen, M. Shan, X. Zhao, Q. Chen, H. Dai and
 288 L. Yao, *Acta Biomaterialia*, 2022, **153**, 386-398.
- 289 5. M. Sahlabadi and P. Hutapea, *Bioinspiration & Biomimetics*, 2018, **13**, 036013.
- 290 6. Z. Chen, Y. Lin, W. Lee, L. Ren, B. Liu, L. Liang, Z. Wang and L. Jiang, ACS
 291 applied materials & interfaces, 2018, 10, 29338-29346.
- J. Ling, Z. Song, J. Wang, K. Chen, J. Li, S. Xu, L. Ren, Z. Chen, D. Jin and L.
 Jiang, *Journal of the mechanical behavior of biomedical materials*, 2017, 68, 173-179.
- 295 8. J. Černý, F. Weyda, M. Perlík and D. Kodrík, *Microscopy and Microanalysis*,
 296 2022, 28, 1808-1818.
- 297 9. L. Wang, Y. Liu, Y. Yang, Y. Li and M. Bai, *Additive Manufacturing*, 2021, 42, 101992.
- D. Han, R. S. Morde, S. Mariani, A. A. La Mattina, E. Vignali, C. Yang, G.
 Barillaro and H. Lee, *Advanced Functional Materials*, 2020, **30**, 1909197.
- S. Y. Yang, E. D. O'Cearbhaill, G. C. Sisk, K. M. Park, W. K. Cho, M. Villiger,
 B. E. Bouma, B. Pomahac and J. M. Karp, *Nature communications*, 2013, 4,
 1702.
- 304 12. Y. Ni, H. Bai, Z. Wang, H. Liao and W. Wu, *Composite Structures*, 2023, 117220.
- J. Rivera, M. S. Hosseini, D. Restrepo, S. Murata, D. Vasile, D. Y. Parkinson, H.
 S. Barnard, A. Arakaki, P. Zavattieri and D. Kisailus, *Nature*, 2020, 586, 543-548.