# **Supplementary Information for**

# **Evaluation of Drug Release from Polymeric Nanoparticles in Simulated Saliva and Gastric Media by Asymmetric Flow Field–Flow Fractionation (AF4)**

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# **S1. Literature Review**

Table S1 provides an overview of the applications of asymmetric flow field–flow fractionation (AF4) for nanocarrier analysis.

**Table S1. Summary of nanocarrier studies using AF4**

Sample (Drug in	<b>AF4 Method</b>		<b>Experimental Design</b>		<b>Reference</b>
<b>Polymeric Carrier)</b>	<b>Nanocarrier</b>	Nanocarrier-associated	<b>Sample Media</b>	<b>Release Study</b>	
	<b>Characterization</b>	<b>Drug Detection</b>			
mRNA in DOTMA and	SAXS: LPX structure;	UV: mRNA quantification;	Aqueous media	N/A	
DOPE liposome	DLS: LPX $R_h$ ;	DLS: mRNA $R_h$ ;			
	MALS: LPX $R_{\rm g}$ , MW	MALS: mRNA $R_{\rm g}$ , MW			
Quercetin-loaded nano-	UV: liposome	N/A	Milli-Q water	N/A	$\overline{2}$
liposome	concentration;				
	MALS: $R_{\rm g}$ , shape				
	factor;				
	DLS: R <sub>h</sub>				
Mitotane liposomes	UV: MT concentration;	Off-line HPLC-DAD:	Purified water	N/A	$\overline{3}$
(DOPC-MT) and albumin-	MALS: BSA-MT $R_{\rm g}$	DOPC-MT and BSA-MT			
stabilized MT nanoparticles					
$(BSA-MT)$					
Pb-DTPA in	UV/RI: Liposome	$\gamma$ -ray: quantification of Pb	Aqueous media	N/A	$4 *$
DSPC/cholesterol/DSPE-	concentration:	and radioactive decay	with NaCl,		
<b>DTPA</b> liposomes	MALS: Liposome $R_{\rm g}$	products from the liposomes,	HEPES and		
		and the size	$DTPA$ (pH 7.4)		
Amphotericin B in	AF4-UV: Separation	Offine HPLC-UV-CAD:	Diluted with 5%	N/A	$\overline{5}$ *
liposomes		quantification of	dextrose solution		
		Amphotericin B,			
		Cholesterol, DSPG and			
		<b>HSPC</b>			
Doxorubicin in liposome	AF4: Separation	Offline LC-MS:	N/A	N/A	$6*$
	Offline NTA/DLS: $Rh$	Doxorubicin concentration	(commercial		
			products)		
p-THPP in liposomes	UV: liposome	Offline HPLC-UV: p-THPP	<b>TRIS</b> buffer	N/A	$7 *$
	concentration;	concentration			
	MALS: liposome $R_{\rm g}$				







\*Note: Asterisks indicate articles before 2021 already summarized in the review article by Quattrini et al.,  $27$ .

index; N/P:  $[-NH_3^+]/[-PO_4^-]$  molar charge ratios; Shape factor:  $(\rho = R \rho R)$ ; Mb: Myoglobin; PEG-b-(PDEAEMA-co-PDMAEMA-co-PDMIBMA: **Abbreviations:** mRNA: messenger RNA; DOTMA: (R)-N,N,N-trimethyl-2-3-dioleyloxy-1-propanaminium chloride; DOPE: 1,2-dioleoyl-snglycero-3-phosphoethanolamine; N/A: not available; SAXS: small angle X-ray scattering; LPX: lipoplex; DLS: Dynamic light scattering; Rh: hydrodynamic radius; MALS: multi angle light scattering;  $R_g$ : radius of gyration; Mw: molecular weight; UV: UV-Vis spectroscopy; RI: refractive poly(ethylene glycol)-b-(poly(diethylaminoethyl methacrylate)-co-poly(dimethylmaleimidobutyl methacrylate)); RB: Rose Bengal; Polymersome: Psome; PBS: Phosphate Buffered Saline; MT: Mitotane; DOPC: 1,2-dioleoyl-sn-glycero-3-phosphocholine; BSA: Bovine serum albumin; CRISPR-Cas9: clustered regularly interspaced short palindromic repeats (CRISPR) associated (Cas); RNP: ribonucleoprotein; LNP: lipid nanoparticle; DiI: 1,1′-dioctadecyl-3,3,3′,3′-tetramethyl-indocarbocyanine perchlorate; IR780: 2-[2-[2-chloro-3-[(1,3-dihydro-3,3-dimethyl-1-propyl-2H-indol-2 ylidene)ethylidene]-1-cyclohexen-1-yl]ethenyl]-3,3-dimethyl-1-propylindolium iodide: Nanosphere: NS; nanocapsule: NC; Dulbecco's Modified Eagle Medium: DMEM; FBS: Fetal bovine serum; DSPC: Diethylenetriamine-N,N,N′,N′′,N′′-pentaacetic acid; DSPC: 1,2-Distearoyl-sn-glycero-3 phosphorylcholine; DSPE: 1,2-Distearoyl-sn-glycero-3-phosphoethanolamine; HEPES: 2-[4-(2-hydroxyethyl)piperazin-1-yl]ethanesulfonic acid; PLA: poly(D,L-lactide); PLA-PEG: polyethylene glycol-block-poly(D,L-lactide); PLA-Cs: PLA with chitosan; AlClPc: [chloro(29H,31Hphthalocyaninato)aluminium; DSPG: 1,2-Distearoyl-sn-3-phosphoglycerol; HSPC: hydrogenated soy L-alpha-phosphatidylcholine; CLZ: Clofazimine; NTA: Nanoparticle tracking analysis; QELS: quasi-elastic light scattering; TRIS: (Tris(hydroxymethyl) aminomethane; RB: Rose Bengal; p-THPP: porphyrin 5,10,15,20-tetrakis(4-hydroxyphenyl)21H,23H-porphine; Egg-PC: Egg-phosphatidylcholine.

#### **S2. PLGA-Enro NP Synthesis**

An organic solution was prepared with 420 mg of PLGA and 39 mg of enrofloxacin, which were dissolved in 10 mL of ethyl acetate by stirring for 30 min at 400 to 500 rpm. An aqueous surfactant solution was prepared by dissolving 550 mg of Tween 80 in 110 mL of low resistivity water. An emulsion was prepared by adding the organic phase to the aqueous phase with stirring (400 to 500 rpm). The sample was then processed in a microfluidizer (M 110P, Microfluidics, Westwood, MA, USA) with four passes. The organic solvent was removed by rotary evaporation (Buchi R-300, Buchi Corp., New Castle, DE, USA) under vacuum at 32 ° C for 70 min. An aqueous PVA solution was prepared using 180 mg PVA in 9 mL of water and added to the NP suspension. Finally, 1189 mg of trehalose was added as a cryoprotectant, and the NPs were freeze-dried (FreeZone 2.5, Labconco Corp., Kansas City, MO, USA) at –80 ° C for 2 d. The NPs were stored at  $-20$  °C until use.

## **S3. Release Media Preparation**

The media used for the release experiments are reported in Table S2. Chemicals used for media preparation included NaCl (ACS grade, VWR Chemicals, Solon, OH, USA), KCl (ACS grade, EMD Millipore, Billerica, MA, USA), Na<sub>2</sub>HPO<sub>4</sub>•7H<sub>2</sub>O (ACS grade, VWR Chemicals, Solon, OH, USA), KH2PO<sup>4</sup> (ACS grade, Amresco, Solon, OH, USA), HCl (ACS grade, Sigma Aldrich, St. Louis, MO, USA),  $\alpha$ -amylase (from porcine pancreas, Type VI-B,  $\geq$  5 units/mg solid, Sigma Aldrich, St. Louis, MO, USA), and pepsin (from porcine gastric mucosa,  $\geq 250$  units/mg solid, Sigma Aldrich, St. Louis, MO, USA).





\*The simulated saliva and SGF were prepared and tested with or without the protein

#### **S4. Batch Total Organic Carbon (TOC) Analysis for Protein Loss in Filtration**

Simulated saliva containing amylase and SGF containing pepsin were filtered prior to use. The protein concentrations in the unfiltered and filtered samples were compared by batch TOC analysis using the grab method measurement mode (Sievers M9 SEC, Suez Water Technologies, Trevose, PA, USA). The samples were diluted in deionized water by a dilution factor of 160 prior to analysis. The TOC analyzer was set to draw sample continuously at 0.5 mL/min, with a 10 min initial flush time followed by five replicate measurements of 2 min duration. Phosphoric acid (6 M) was injected at 2.0 μL/min for inorganic carbon removal, and a buffered ammonium persulfate solution (150 g/L in phosphate buffer) was injected at 13.0 μL/min to oxidize organic carbon to CO<sup>2</sup> for detection. The signals for the last 3 measurement replicates were averaged per sample, with triplicate samples prepared and analyzed for each unfiltered and filtered protein solution.

# **S5. Drug Release at 37 °C**

Figure S1 compares the drug release at 37 °C in the various media. The same trend was observed across all five media as in the experiments at 30 °C, but the rapid rate of release and nearly-complete release in the SGF media by 2 hours introduces uncertainty in the release time points, as some time is required to collect sample out of the heated bath and perform the AF4 analyses. Hence, all other experiments were conducted at 30 °C, where slower release is achieved and there is lower relative uncertainty in the sampling time points.



**Figure S1.** Drug release profiles and radial diffusion model fits for PLGA-Enro NPs in various release media at 37 °C for up to 8 hours. Preliminary data were collected on single experiments.

#### **S6. AF4 Method Details**

The AF4 method for the PLGA-Enro NPs was applied using the settings optimized in our prior method development study.<sup>[28](#page-18-4)</sup> Table S3 presents the AF4 separation method, i.e., focus flow and crossflow settings and durations. The detector flow rate was 0.5 mL/min throughout the entire measurement run. During the sample injection steps, the injection flow rate was 0.2 mL/min.

<b>Mode</b>	<b>Duration</b> (min)	Crossflow rate (mL/min)
Elution	6	0.15
Focus		1.5
$Focus + Injection$	4	1.5
Elution	58	0.15
$Elution + Injection$	15	$\theta$
Elution	6	$\theta$
Elution	10	0.15

**Table S3**. Crossflow rates and duration of each separation step in the AF4 method

The online detectors connected to the AF4 effluent were ordered as (1) UV diode array detector (DAD), (2) multi-angle light scattering (MALS) / dynamic light scattering (DLS) detector, (3) fluorescence detector (FLD), (4) differential refractive index (dRI) detector, and (5) total organic carbon (TOC) detector, following the pressure limits (high to low) of each detector and the destructive nature of the TOC analysis. Bovine serum albumin (BSA) was run as a calibration standard in a buffer comprised of 4 mM phosphate and 25 mM NaCl (pH  $\approx$  7) with the same detector flow (0.5 mL/min) and a higher crossflow during the focus and elution stages (2.0 mL/min). The BSA was used for detector alignment, band broadening correction, and MALS detector normalization.

#### **S7. Additional Release Models**

Two additional release models were applied to the drug release data for comparison against the radial diffusion model:

#### *(a) First-order kinetic model:*

$$
\frac{M_{\text{released}}}{M_{\text{total}}} = 1 - \exp(-k \frac{t}{\text{first order}})
$$
\n(S1)

This model predicts the fraction of drug mass released ( $M_{\text{released}}/M_{\text{total}}$ ) over time (t) to follow first order kinetics with rate constant *k*first order. The model assumes perfect sink conditions and homogeneous drug distribution in the particles at all times. These assumptions are not expected to be representative of the PLGA-Enro nanoparticles, but the model is evaluated for comparison since it is frequently applied to drug release profiles.

(b) Erosion model:<sup>29</sup>  
\n
$$
\frac{M_{\text{released}}}{M_{\text{total}}} = 1 - (1 - k_{\text{erosion}} t)^3
$$
\n(S2)

This model assumes that the drug is homogeneously distributed within the polymer matrix and only releases upon erosion of the particle, i.e., it does not dissolve or diffuse out of the particles. The polymer mass erosion rate (i.e., rate of decrease in the particle volume) is assumed to be proportional to the outer surface area of the spherical particles. The rate constant *k*erosion represents a lumped constant comprising the erosion rate (nm/s) along with geometric factors (relating surface area and volume) and mathematical integration factors. The model was fitted to only the first 90% of drug release, as the cubic model equation above is not limited to a maximum release of 100%.

## **S8. Zeta Potential Results**

The measured zeta potentials of the PLGA-Enro NPs in the various media at the beginning (0 h) and end (48 h) of the release experiments are provided in Figure S2.



**Figure S2.** Measured zeta potentials of the PLGA-Enro NPs between 0 and 48 h in all release experiment conditions tested. Samples were diluted from 15 g/L to 1 g/L of PLGA-Enro NPs (as total lyophilized powder), resulting in an ionic strength and pH of 14.1 mM (pH 7.2) for PBS, 2.3 mM (pH 5.6 to 6.0) for saliva with or without amylase, and 2.9 mM (pH 3.4 to 3.6) for SGF with or without pepsin. Error bars represent standard deviations on triplicated experiments.

### **S9. AF4-TOC Results**

The online TOC detector could be used to quantify the PLGA-Enro NPs. Figure S3 shows an example of the AF4-TOC chromatograms and fluorescent drug release analysis using the TOC signal for NP quantification for PLGA-Enro NPs in SGF without pepsin at 30 °C. Because the samples contained excess polyvinyl alcohol surfactant in the NP formulation (and biomolecules in the media containing proteins), a large void peak corresponding to these species appears in the AF4-TOC chromatograms, complicating the analysis of the NP peak by TOC detection.



**Figure S3**. AF4-TOC chromatograms for quantifying PLGA NPs (a), AF4-FLD chromatograms for quantifying enrofloxacin loading (left axis of b), and percentages of enrofloxacin remaining at each elution time point (right axis of b). The data were processed as in Figure 2, except using the TOC signal in place of the UV signal. Representative chromatograms are shown for one experiment of a total of three replicates per release media.



**Figure S4.** AF4-UV chromatograms and online DLS measurements (a, c, and e), AF4-FLD analyses (b, d, and f) for enrofloxacin release in media with proteins or at 20 °C. Representative chromatograms are shown for one experiment of a total of three replicates per release media.

# **S11. Model Fitting on the Bulk Drug Release Profiles**

Table S4 provides the best-fit radial diffusion rate constant and diffusion coefficient determined for the PLGA-Enro NPs in each release medium, along with the 95% confidence intervals on the model fits.

<b>Experiment Condition</b>	<b>Fitted Parameters</b> <sup>†</sup>		
	$k$ radial diffusion $(h^{-1})$	$D$ (cm <sup>2</sup> s <sup>-1</sup> )	
PBS, 30 °C	0.0017	$5.0 \times 10^{-17}$	
	(0.0013, 0.0021)	$(3.9, 6.2) \times 10^{-17}$	
	0.0024	$5.9 \times 10^{-17}$	
Saliva without amylase, $30^{\circ}$ C	(0.0021, 0.0029)	$(5.0, 6.9) \times 10^{-17}$	
SGF without pepsin, $30^{\circ}$ C	0.0098	$22 \times 10^{-17}$	
	(0.0087, 0.0109)	$(20, 24) \times 10^{-17}$	
Saliva with amylase, $30^{\circ}$ C	0.0040	$9.3 \times 10^{-17}$	
	(0.0036, 0.0044)	$(8.4, 10.3) \times 10^{-17}$	
	0.0073	$16 \times 10^{-17}$	
SGF with pepsin, 30 $\degree$ C	(0.0064, 0.0083)	$(14, 18) \times 10^{-17}$	
SGF without pepsin, 20 $^{\circ}$ C	0.00005	$0.13 \times 10^{-17}$	
	(0.00001, 0.00012)	$(0.03, 0.30) \times 10^{-17}$	

**Table S4. Radial Diffusion Model Fitting Parameters for Release in Various Conditions**

**†**Fitted parameters are presented as the best-fit value on the triplicated release experiments, followed by the upper and lower bounds of the 95% confidence interval on the model fit in parentheses.

#### **S12. Evaluation of Drug-Protein Interactions in Solution**

Proteins elute in the void peak during the AF4 measurements of the PLGA-Enro NPs. Hence, drug-protein interactions could be probed by evaluating the enrofloxacin fluorescence signal in the void peak (Figure S5). In control injections of the protein-containing media (without NPs), amylase did not contribute any fluorescence at the excitation/emission wavelengths used for enrofloxacin detection, whereas pepsin did. In all media, the void peak fluorescence was initially high (likely from free enrofloxacin initially present in the NP formulation), but decreased to the background fluorescence signal for the proteins alone over the course of the release experiment. In addition, the rate of free enrofloxacin depletion was similar for protein-containing and proteinfree media. These results suggest that there were no significant drug-protein interactions.



**Figure S5.** Fluorescence void peak areas for the PLGA-Enro NPsin saliva with or without amylase (a) and SGF with or without pepsin (b) at 30 °C, along with fluorescence peak area for control measurements on the proteins in the media (without NPs). Error bars represent standard deviations on triplicate release experiments, and shaded bounds represent standard deviations on triplicate measurements of the pepsin in SGF.

#### <span id="page-16-2"></span><span id="page-16-1"></span><span id="page-16-0"></span>**References**

- <span id="page-16-3"></span>1. M. A. Graewert, C. Wilhelmy, T. Bacic, J. Schumacher, C. Blanchet, F. Meier, R. Drexel, R. Welz, B. Kolb, K. Bartels, T. Nawroth, T. Klein, D. Svergun, P. Langguth and H. Haas, *Sci. Rep.*, 2023, **13**, 15764.
- <span id="page-16-5"></span><span id="page-16-4"></span>2. S. Melchior, M. Codrich, A. Gorassini, D. Mehn, J. Ponti, G. Verardo, G. Tell, L. Calzolai and S. Calligaris, *Food Chem.*, 2023, **428**, 136680.
- <span id="page-16-6"></span>3. C. Langer, M. Köll-Weber, M. Holzer, C. Hantel and R. Süss, *Pharmaceutics*, 2022, **14**, 1891.
- <span id="page-16-8"></span><span id="page-16-7"></span>4. S. Huclier-Markai, A. Grivaud-Le Du, E. N'tsiba, G. Montavon, M. Mougin-Degraef and J. Barbet, *J. Chromatogr. A*, 2018, **1573**, 107-114.
- <span id="page-16-9"></span>5. D. Van Haute, W. Jiang and T. Mudalige, *Int. J. Pharm.*, 2019, **569**, 118603.
- 6. S. M. Ansar and T. Mudalige, *Int. J. Pharm.*, 2020, **574**, 118906.
- <span id="page-16-10"></span>7. A. H. Hinna, S. Hupfeld, J. Kuntsche and M. Brandl, *J. Pharm. Biomed. Anal.*, 2016, **124**, 157-163.
- <span id="page-16-11"></span>8. C. Decker, A. Fahr, J. Kuntsche and S. May, *Chem. Phys. Lipids*, 2012, **165**, 520-529.
- 9. A. Hinna, F. Steiniger, S. Hupfeld, M. Brandl and J. Kuntsche, *Anal. Bioanal. Chem.*, 2014, **406**, 7827-7839.
- 10. A. H. Hinna, S. Hupfeld, J. Kuntsche, A. Bauer-Brandl and M. Brandl, *J. Controlled Release*, 2016, **232**, 228-237.
- 11. S. Hupfeld, D. Ausbacher and M. Brandl, *J. Sep. Sci.*, 2009, **32**, 3555-3561.
- 12. G. E. N. Pound-Lana, G. M. Garcia, I. C. Trindade, P. Capelari-Oliveira, T. G. Pontifice, J. M. C. Vilela, M. S. Andrade, B. Nottelet, B. B. Postacchini and V. C. F. Mosqueira, *Mater. Sci. Eng., C*, 2019, **94**, 220-233.
- <span id="page-17-3"></span><span id="page-17-2"></span><span id="page-17-1"></span><span id="page-17-0"></span>13. M. A. de Oliveira, G. Pound-Lana, P. Capelari-Oliveira, T. G. Pontífice, S. E. D. Silva, M. G. C. Machado, B. B. Postacchini and V. C. F. Mosqueira, *J. Chromatogr. A*, 2021, **1641**, 461959.
- 14. S. Hester, K. B. Ferenz, A. Adick, C. Kakalias, D. Mulac, S. Azhdari and K. Langer, *Int. J. Pharm.*, 2023, **646**, 123454.
- <span id="page-17-5"></span><span id="page-17-4"></span>15. M. G. C. Machado, G. Pound-Lana, M. A. de Oliveira, E. G. Lanna, M. C. P. Fialho, A. C. F. de Brito, A. P. M. Barboza, R. D. d. O. Aguiar-Soares and V. C. F. Mosqueira, *Drug Delivery Transl. Res.*, 2020, **10**, 1626-1643.
- <span id="page-17-8"></span><span id="page-17-7"></span><span id="page-17-6"></span>16. L. T. Oliveira, M. A. de Paula, B. M. Roatt, G. M. Garcia, L. S. B. Silva, A. B. Reis, C. S. de Paula, J. M. C. Vilela, M. S. Andrade, G. Pound-Lana and V. C. F. Mosqueira, *Eur. J. Pharm. Sci.*, 2017, **105**, 19-32.
- <span id="page-17-9"></span>17. Y. Hu, R. M. Crist and J. D. Clogston, *Anal. Bioanal. Chem.*, 2020, **412**, 425-438.
- 18. J. Walther, D. Wilbie, V. S. J. Tissingh, M. Öktem, H. van der Veen, B. Lou and E. Mastrobattista, *Pharmaceutics*, 2022, **14**, 213.
- <span id="page-17-10"></span>19. W. Fraunhofer, G. Winter and C. Coester, *Anal. Chem.*, 2004, **76**, 1909-1920.
- 20. A. Sajid, M. Castronovo and F. M. Goycoolea, *Polymers*, 2023, **15**, 2115.
- 21. M. Palinske, U. L. Muza, S. Moreno, D. Appelhans, S. Boye, R. Schweins and A. Lederer, *Macromol. Chem. Phys.*, 2023, **224**, 2200300.
- 22. K. Sztandera, M. Gorzkiewicz, X. Wang, S. Boye, D. Appelhans and B. Klajnert-Maculewicz, *Colloids Surf., B*, 2022, **217**, 112662.
- 23. J. Wankar, F. Bonvicini, G. Benkovics, V. Marassi, M. Malanga, E. Fenyvesi, G. A. Gentilomi, P. Reschiglian, B. Roda and I. Manet, *Mol. Pharmaceutics*, 2018, **15**, 3823- 3836.
- <span id="page-18-3"></span><span id="page-18-2"></span><span id="page-18-1"></span><span id="page-18-0"></span>24. A. Moquin, J. Ji, K. Neibert, F. M. Winnik and D. Maysinger, *ACS Omega*, 2018, **3**, 13882-13893.
- 25. J. Ehrhart, A.-F. Mingotaud and F. Violleau, *J. Chromatogr. A*, 2011, **1218**, 4249-4256.
- 26. S. Boye, N. Polikarpov, D. Appelhans and A. Lederer, *J. Chromatogr. A*, 2010, **1217**, 4841-4849.
- 27. F. Quattrini, G. Berrecoso, J. Crecente-Campo and M. J. Alonso, *Drug Delivery Transl. Res.*, 2021, **11**, 373-395.
- <span id="page-18-4"></span>28. S. Shakiba, C. E. Astete, R. Cueto, D. F. Rodrigues, C. M. Sabliov and S. M. Louie, *J. Controlled Release*, 2021, **338**, 410-421.
- <span id="page-18-5"></span>29. J.-M. Vergnaud, *Controlled Drug Release of Oral Dosage Forms*, Ellis Horwood, New York, NY, 1993.